21 24 L 21 Sign F38

(19) Japanese Patent Office

(12) Publication of Unexamined Patent Applications (A)

(11) Unexamined Patent Application Number

Unexamined Patent Application H11-155812

(43) Publication Date: June 15, Heisei 11 (1999)

(51) Int.Cl.6		Identification Symbol	F I			
A 6 1 B	1/06		A 6 1 B	1/06	В	
	1/06	3 0 0		1/06	3 0 0 F	

Request for Examination: Examination not requested Number of Claims: 1 OL (9 pages total)

(21) Application Number	Patent Application 9-331991	(71) Applicant	00000376
] ' ' ''	Olympus Optical Co. Ltd.
(22) Application Date	December 2, Heisei 9 (1997)		2-43-2 Hatagaya, Shibuya-ku, Tokyo
. ,	, , ,	(72) Inventor	Isami HIRAO
			at Olympus Optical Co. Ltd.
			2-43-2 Hatagaya, Shibuya-ku, Tokyo
		(72) Inventor	Nobuyuki MICHIGUCHI
			at Olympus Optical Co. Ltd.
			2-43-2 Hatagaya, Shibuya-ku, Tokyo
	•	(72) Inventor	Mamoru KANEKO
			at Olympus Optical Co. Ltd.
			2-43-2 Hatagaya, Shibuya-ku, Tokyo
		(74) Agent	Susumu ITO, Attorney
•			Continued on last pag

(54) [Title of Invention] FLUORESCENT OBSERVATION DEVICE

[Problem to be Solved] To observe a lesion existing at a depth inside an organism.

[Solution] A fluorescent observation device 1 includes an optical probe 3 formed from a needle sheath 2 which is rigid only at the tip inserted into the organism, and flexible at others; an excitation light source 4 which supplies excitation light for fluorescent observation to optical probe 3; a controller 5 which controls the supply of the excitation light from the excitation light source 4 to the optical probe 3; and a spectrometer 6 for diagnosing a tissue using autofluorescence from a lesion at a depth in the organism caused by excitation light from the optical probe 3. A first conduit 7 and a second conduit 8 are formed in the interior of needle sheath 2 of optical probe 3, and a first fiber-optic cable 9 is distributed in first conduit 7 to transmit the auto-fluorescence from the lesion at a depth of the organism to the spectrometer 6; as is a second fiber-optic cable 10 in second conduit 8 to transmit the excitation light from excitation light source 4.

[Diagram]

- 4. Excitation light source
- 5. Controller
- 6. Spectrometer

[Claim(s)]

[Claim 1] In relation to fluorescent observation devices for illuminating organic tissue with excitation light to makes observations of said organic tissue by the fluorescent light emitted by said organic tissue,

a fluorescent observation device characterized by being equipped with

a needle-shaped sheath inserted deep into organic tissue,

and an ultrasonic observation instrument used to confirm the insertion condition of said needle-shaped sheath in said deep organic tissue.

and having an irradiative fiber-optic cable for transmitting said excitation light and an observational fiber-optic cable for transmitting the fluorescent light emitted by said organic tissue formed through the interior of said needle-shaped sheath.

[Description of the Invention]

[0001]

[Technological Field of the Invention] The present invention is associated with fluorescent observation devices which irradiate the test subject with excitation light so that diseased parts can be observed using the fluorescence emitted by the test subject; more specifically, it is associated with fluorescent observation devices with a characteristic in the part that irradiates the test subject with excitation light.

[0002]

[Prior Art] In recent years, there has been increasing use of technology in which the observational target area of organic tissue is irradiated with excitation light, and the auto-fluorescence emitted directly by the organic tissue due to excitation light, or the fluorescence of a substance injected into the organism, is extracted as a 2-dimensional image, and diagnoses of degradation of organic tissue and the condition of diseases such as cancer (for example, the type of disease and the extent of infiltration) are made from this fluorescence image. As shown in Publication of Unexamined Patents Number H8-252218, for example, a variety of fluorescent observation devices for conducting this fluorescence observation have been proposed.

[0003] Auto-fluorescence occurs when biological tissue irradiated with excitation light emits fluorescent light with wavelength longer than that of the excitation light. Examples of biological matter capable of florescence include collagen, NADH (nicotinamide adenine dinucleotide), FMN (flavin mononucleotide), and pyridine nucleotide. Nowadays, it is possible to diagnose diseases such as cancer through fluorescence, as there is a clearer understanding of the

correlation between diseases and the fluorescence of internal biological matter.

[0004] In the case of fluorescent pharmaceuticals, HpD (hematoporphyrin), Photofrin, and ALA (\delta-amino levulinic acid), for example, are used as fluorescent substances injected into the organism. These pharmaceuticals tend to accumulate in cancerous cells; hence the diseased area can be diagnosed by injecting these substances into the body and examining the fluorescent areas. In another method, fluorescent substances are attached to monoclonal antibodies, and the fluorescent substances accumulate in the diseased area through antigen-antibody reactions.

[0005] As excitation light, lasers, mercury lamps, and metal halide lamps, for example, are used, and by irradiating organic tissue with excitation light, fluorescence images of the observational target areas are obtained. Observations and diagnoses are conducted by extracting the weak fluorescent light emitted by the organic tissue due to excitation light and producing a 2-dimensional fluorescence image.

[0006]

[Problem to be Solved] The problem, however, is that in existing fluorescent observation devices described in the Publication of Unexamined Patents Number H8-252218, an organism's surface tissue is irradiated with excitation light, and the auto-fluorescence emitted from the organism's surface tissue is observed endoscopically, so that only lesions existing on the surface of the organism can be observed, and lesions existing at a depth inside the organism cannot be observed.

[0007] The present invention was created in response to the conditions outlined above, and has the objective of providing a fluorescent observation device capable of observing lesions that exist at a depth inside an organism.

[8000]

[Solution] In relation to fluorescent observation devices for illuminating organic tissue with excitation light to makes observations of said organic tissue by the fluorescent light emitted by said organic tissue, the fluorescent observation device of the present invention is equipped with a needle-shaped sheath inserted deep into organic tissue and an ultrasonic observation instrument used to confirm the insertion condition of said needle-shaped sheath in said deep organic tissue, and has an irradiative fiber-optic cable for transmitting said excitation light and an observational fiber-optic cable for transmitting the fluorescent light emitted by said organic tissue formed through the interior of said needle-shaped sheath.

[0009] The fluorescent observation device of this invention allows observation of lesions existing at a depth inside an organism by inserting said needle-shaped sheath in said deep organic tissue, confirming the insertion condition of said needle-shaped sheath in said deep organic tissue using said ultrasonic observation instrument, and at the same time, transmitting said excitation light to said organic tissue through said irradiative fiber-optic cable, and transmitting the fluorescent light emitted from said organic tissue using said observational fiber-optic cable.

[0010]

[Embodiments of the Invention] The embodiments of this invention will be explained below with reference to drawings.

[0011] (First Embodiment) Figure 1 to Figure 3 are associated with the first embodiment of this invention. Figure 1 is a schematic diagram showing the constitution of the fluorescent observation device, Figure 2 is a schematic diagram showing the constitution of the convex ultrasonic endoscope, used in the fluorescent observation device, through which the optical probe in Figure 1 is inserted, and Figure 3 shows the monitor used to display the ultrasonic image obtained by the convex ultrasonic endoscope of Figure 2.

[0012] (Constitution) As shown in Figure 1, the fluorescent observation device 1 of the present embodiment includes an optical probe 3 consisting of a needle-shaped sheath 2 which is flexible except at the rigid tip which is inserted into the organism; an excitation light source 4 which supplies the excitation light used for

fluorescence observation to optical probe 3; a controller 5 which controls the supply of the excitation light from excitation light source 4 to optical probe 3; and a spectrometer 6 which is used to diagnose tissue using the auto-fluorescence emitted by a lesion at a depth in the organism due to the excitation light from optical probe 3.

[0013] A first conduit 7 and a second conduit 8 are formed in the interior of needle-shaped sheath 2 of optical probe 3, and a first fiber-optic cable 9 connected to spectrometer 6 is distributed in first conduit 7 to transmit the auto-fluorescence from the lesion at a depth of the organism to spectrometer 6, as is a second fiber-optic cable 10 in second conduit 8 to transmit the excitation light from excitation light source 4.

[0014] As shown in Figure 2, optical probe 3 is inserted within conduit 16 of convex ultrasonic endoscope 15, which is equipped with ultrasonic receiver 14 with ultrasonic vibrators positioned in a convex arc in toward the insertion direction in relation to objective optic module 13 formed inside tip 11 to make optical observations of organic tissue 12. In fluorescent observation device 1, convex ultrasonic endoscope 15, not shown, is connected to the observational light source which supplies observational illumination and to the ultrasonic observation device which transmits ultrasound via ultrasonic receiver 14 and generates an ultrasonic image; and is constituted such that it is possible to confirm the condition of the insertion of optical probe 3 in organic tissue 12, for example by observing the optical image of organic tissue 12 in the body cavity through an ocular unit while displaying the ultrasonic image from the ultrasonic observation device on an external monitor as shown in Figure 3.

[0015] (Operation) Next, the operation of fluorescent observation device 1 constituted according to the present embodiment will be explained.

[0016] Optical probe 3 of fluorescent observation device 1 is inserted into organic tissue 12 via conduit 16 of convex ultrasonic endoscope 15. At this time, the ultrasonic image at a depth in organic tissue 12 is displayed on external monitor 17 connected to convex ultrasonic endoscope 15, and the operator guides optical probe 3 while confirming that optical probe 3 is securely inserted in lesion 18 deep inside organic tissue 12 (refer to Figure 3).

[0017] Then, when the operator confirms that optical probe 3 has been inserted securely into targeted lesion 18 deep inside organic tissue 12, the operator manipulates the externally installed controller 5, so that the excitation light is transmitted from excitation light source 4 to lesion 18, and this excitation light is irradiated onto lesion 18 deep inside organic tissue 12 via second fiber-optic cable 10.

[0018] When lesion 18 deep inside organic tissue 12 is irradiated by the excitation light, it emits auto-fluorescence, and the auto-fluorescence is guided into the externally installed spectrometer via first fiber-optic cable 9. Then, by reading spectrometer 6, the operator conducts fluorescence observation of lesion 18 deep inside organic tissue 12.

[0019] (Effects) In this embodiment of fluorescent observation device 1, the fluorescence from not only the surface of organic tissue 12, but from lesion 18 deep inside organic tissue 12, can be observed by inserting optical probe 3 in lesion 18 at a depth in organic tissue 12. Also, because the insertion condition of optical probe 3 deep inside organic tissue 12 is observed by convex ultrasonic endoscope 15, the operator can insert the optical probe securely in lesion 18.

[0020] Also, in this embodiment, convex ultrasonic endoscope 15 is used to confirm the insertion position of optical probe 3, but the insertion position of optical probe 3 can be confirmed by radial or linear ultrasonic endoscopes as well before conducting fluorescence observation of lesion 18 deep inside organic tissue 12.

[0021] (Second Embodiment) Figure 4 is a schematic diagram showing the constitution of the fluorescent observation device associated with the second embodiment of the present invention.

[0022] The second embodiment is almost identical to the first embodiment, so only the differences will be explained, and where the

constitution is identical, the same symbols will be used, and explanations will be omitted.

[0023] (Constitution) As shown in Figure 4, in fluorescent observation device 1a of the present embodiment, a third conduit 21, in addition to a first conduit 7 and a second conduit 8, is formed inside a needle-shaped sheath 2 of an optical probe 3, and this third conduit 21 is connected to syringe 24 and 25 installed in the exterior to allow injections of pharmaceutical 22 used in fluorescent diagnosis and therapeutic pharmaceutical 23, such that by controlling valve 26, each can be selectively supplied to third conduit 21.

[0024] Also, fluorescent observation device 1a of the present embodiment includes therapeutic light source 27, and uses controller 5 to selectively irradiate/supply excitation light from excitation light source 4 or light from therapeutic light source 27 to second fiberoptic cable 10 formed inside second conduit 8.

[0025] Additionally, hematoporphyrin (HPD) for example can be used as pharmaceutical 22 used in fluorescent diagnosis, and lumin for example can be used as therapeutic pharmaceutical 23.

[0026] The remaining constitution is identical to that of the first embodiment.

[0027] (Operation) Optical probe 3 in this embodiment of fluorescent observation device 1a is, as in the first embodiment, inserted deep inside organic tissue 12 via conduit 16 of convex ultrasonic endoscope 15 (refer to Figure 2). Then, while observing the ultrasonic image from convex ultrasonic endoscope 15 on external monitor 17, optical probe 3 is guided into lesion 18 deep inside organic tissue 12.

[0028] When the operator confirms that optical probe 3 has been inserted into lesion 18 deep inside organic tissue 12, the operator controls valve 26, and injects pharmaceutical 22 used for fluorescent diagnosis from syringe 24 into lesion 18 via third conduit 21. Next, through controller 5, a diagnostic excitation light from diagnostic excitation light source 4 is irradiated onto lesion 18 deep inside organic tissue 12 via second fiber-optic cable 10.

[0029] When this happens, pharmaceutical 22 for fluorescent diagnosis has been injected into lesion 18, so lesion 18 emits fluorescent light. This fluorescent light is guided into externally installed spectrometer 6 via first fiber-optic cable 9 installed inside first conduit 7. Diagnosis of fluorescence from lesion 18 then becomes possible as the operator observes spectrometer 6.

[0030] After the observation of lesion 18 deep inside organic tissue 12 is finished, next, therapeutic pharmaceutical 23 from externally installed syringe 25 is injected into lesion 18 deep inside organic tissue 12 via third conduit 21. Then, the therapeutic light from externally installed therapeutic light source 23 is guided into second fiber-optic cable 10 via controller 5.

[0031] When this happens, the therapeutic light is emitted from optical probe 3 causes a chemical reaction with therapeutic pharmaceutical 23, and treats lesion 18 deep inside organic tissue 12. [0032] (Effects) In this embodiment of fluorescent observation device 1a, in addition to the effects of the first embodiment, the treatment of lesion 18 deep inside organic tissue 12 is made possible. [0033] (Third Embodiment) Figure 5 is a schematic diagram showing the constitution of the fluorescent observation device associated with the third embodiment of the present invention.

[0034] The third embodiment is almost identical to the first embodiment, so only the differences will be explained, and where the constitution is identical, the same symbols will be used, and explanations will be omitted.

[0035] (Constitution) As shown in Figure 5, in the present embodiment of fluorescent observation device 1b, a third conduit 31, in addition on a first conduit 7 and a second conduit 8, is formed inside a needle-shaped sheath 2 of an optical probe 3, and this third conduit 31 is connected to a syringe 31 which is installed externally such that therapeutic pharmaceutical 32 can be injected.

[0036] Also, the present embodiment of fluorescent observation device 1b is constituted such that the auto-fluorescent light from lesion 18 deep inside organic tissue 12 transmitted through first fiber-

optic cable 9 installed inside first conduit 7 is imaged by a highsensitivity camera with a built-in image intensifier, the signal is processed by image processor 25, and the fluorescence image of lesion 18 can be observed by an operator using monitor 36.

[0037] Here, the excitation light source 4 controlled by controller 5 uses, for example, helium-cadmium lasers, and the wavelength of the excitation light is 442 nm. Also, titanium oxide (TiO₂) is used as therapeutic pharmaceutical 32.

[0038] The remaining constitution is identical to that of the first embodiment.

[0039] (Operation) Optical probe 3 in this embodiment of fluorescent observation device 1b is, as in the first embodiment, inserted deep inside organic tissue 12 via conduit 16 of convex ultrasonic endoscope 15 (refer to Figure 2). Then, while observing the ultrasonic image from convex ultrasonic endoscope 15 on external monitor 17, optical probe 3 is guided into lesion 18 deep inside organic tissue 12.

[0040] Then, the operator confirms that optical probe 3 has been inserted into lesion 18 deep inside organic tissue 12, and when the insertion into lesion 18 deep inside organic tissue 12 has been confirmed, the 442 nm excitation light used for fluorescence observation is supplied by the externally installed excitation light source.

[0041] This excitation light is irradiated onto Jegion 18 deep inside organic tissue 12 via second fiber-optic cable 10. When irradiated by the 442 nm excitation light, auto-fluorescence is emitted from deep inside organic tissue 12. This auto-fluorescence is captured by the externally installed high-sensitivity camera 34 via first fiber-optic cable 9, is processed by image processor 35, and lesion 18 is displayed as a fluorescence image on externally installed monitor 36. [0042] Once the operator has confirmed lesion 18 using monitor 36, the operator next injects lesion 18 deep inside organic tissue 12 with TiO2, the externally installed therapeutic pharmaceutical 32, via third conduit 31. Then, the operator irradiates lesion 18 deep inside organic tissue 12 with the 442 nm light from excitation light source 4 consisting of a helium-cadmium laser via second fiber-optic cable 10. Because TiO₂ of therapeutic pharmaceutical 36 has been injected deep inside organic tissue 12, the 442nm light emitted by the excitation light source 4 causes an oxidation-reduction reaction, and treats lesion 18 deep inside organic tissue 12.

[0043] (Effects) In this embodiment of fluorescent observation device 1b, as in the second embodiment and in addition to the effects of the first embodiment, the treatment of lesion 18 deep inside organic tissue 12 is made possible. Also, compared to the second embodiment, one light source acts as both the therapeutic light source and the diagnostic light source, which allows a reduction in the size of the design. Additionally, diagnostic capabilities are increased because information from deep inside organic tissue 12 is displayed as an image.

[0044] (Fourth Embodiment) Figure 6 is a schematic diagram showing the constitution of the fluorescent observation device associated with the fourth embodiment of the present invention.

[0045] (Constitution) As shown in Figure 6, fluorescent observation device 51 of the present embodiment includes endoscope 54 possessing an MR antenna 54 inside the tip of insertion unit 52 which is inserted inside the body cavity of the subject; a light source 56a which supplies excitation light used for fluorescence observation to endoscope 54 and a light source 56 equipped with amplifier 55 which amplifies the MR signal from MR antenna 53; a highsensitivity camera 57, with a built-in intensifier, which images the auto-fluorescent light emitted by the organic tissue stimulated by the excitation light used for fluorescence observation; an MR image processor 58 in which a subject placed in a static magnetic field, and a high-frequency magnetic field is generated using MR antenna 53, and at the same the MR signal from MR antenna 53, amplified by amplifier 55, is used to generate an MR image; and a fluorescence image processor 59 which produces a fluorescence image from the image signal imaged by high-sensitivity camera 57, and is configured

such that it displays the MR image and fluorescence image produced by MR image processor 58 and fluorescence image processor 59 on monitor 60.

[0046] In endoscope 54, a removable universal cable 62 stretches out from grip 61, formed at the end of insertion unit 52, such that it can be attached and removed from light source 56, and configured such that the excitation light for fluorescence observation from light source 56 is transmitted through light guide 63 which runs through the interior of universal cable 62 and insertion unit 52, and is irradiated onto the organic tissue from the tip of endoscope 54.

[0047] Also, a signal line 64 connected to MR antenna 53 is distributed inside universal cable 62 and insertion unit 52, and configured such that the detection signal from MR antenna 53 is transmitted by this signal line 64 to the amplifier inside light source 56.

[0048] Furthermore, an image guide 65 is formed inside insertion unit 52 and grip 61, and is configured such that the auto-fluorescence from the organic tissue stimulated by the excitation light for fluorescence observation is relayed to removable ocular unit 66 connected to high-sensitivity camera 57.

[0049] (Operation) Next, the operation of fluorescent observation device 51 constituted as in the present embodiment is explained.

[0050] The subject is placed in a static magnetic field, and insertion unit 52 of endoscope 54 is inserted into the body cavity. Then, the excitation light for fluorescence observation is shone out from light source 56, and the excitation light is irradiated, from the tip of endoscope 54 via light guide 63, onto the organic tissue. When the organic tissue is irradiated by the excitation light, auto-fluorescent light is emitted by the organic tissue, and this auto-fluorescent light is sent to high-sensitivity camera 57 via image guide 65. Then, external fluorescence image processor 59 processes the image, and monitor 60 displays the fluorescence image.

[0051] Also, a high-frequency signal at a prescribed frequency is sent from MR image processor 58 to MR antenna 53 built into endoscope 54, and a high-frequency magnetic field is generated from MR antenna 53 onto the subject. Additionally, the direction of the high-frequency magnetic field that is perpendicular to the direction of the static magnetic field is desirable. Then, the MR signal from the subject is received by MR antenna 53, amplified by amplifier 55, and information along the depth of the lesion being observed fluorescently is obtained. This signal is guided into MR image processor 58, and is displayed on monitor 60 as an MR image.

[0052] As a result, the operator makes observations of the organism's surface and along its depth by the fluorescence image and MR image displayed on monitor 60.

[0053] (Effects) In this embodiment of fluorescent observation device 51, information about the lesion's surface can be observed as a fluorescence image, and also, because information along the depth of the lesion can be observed as an MR image, not only information about the organism's surface, but information along the depth of the organism can be observed, resulting in an increase in diagnostic capabilities.

[0054] (Fifth Embodiment) Figure 7 and Figure 8 are associated with the fifth embodiment of the present invention. Figure 7 is a schematic diagram showing the constitution of the optical probe of the fluorescent observation device, and Figure 8 is a schematic diagram showing the constitution of the endoscope with the optical probe in Figure 7 inserted through the conduit.

[0055] The fifth embodiment is almost identical to the fourth embodiment, so only the differences will be explained, and where the constitution is identical, the same symbols will be used, and explanations will be omitted.

[0056] The fourth embodiment includes an endoscope with an MR antenna installed inside the tip, but in this embodiment, the fluorescent observation device is configured with an ordinary endoscope through which an optical probe, equipped with an MR antenna, is inserted.

[0057] Namely, as shown in Figure 7, optical probe 71 of the present embodiment is equipped with a built-in image guide 72 which transmits the fluorescence image from the organic tissue; and a first MR antenna 73 formed around the exterior circumference, and a second MR antenna 74 formed along the direction of insertion, of image guide 72 for observing information at a depth in the organism. [0058] Then, as shown in Figure 8, an optical probe 71 is inserted in the organism of a properties of the properties of a production of a properties of a properties.

[0058] Then, as shown in Figure 8, an optical probe 71 is inserted in and protruded out the tip of conduit 82 of endoscope 81 which is inserted in the body cavity, and by this, fluorescence images and MR images are obtained.

[0059] In addition, through not shown, [the fifth embodiment is configured] as in the fourth embodiment such that the excitation light for fluorescence observation from light source 56 is supplied to light guide 83 of endoscope 81; image guide 72 of optical probe 71 transmits the fluorescent light from the organic tissue, which is imaged by high-sensitivity camera 57 and processed by fluorescence image processor 59; and furthermore, the MR signals from first MR antenna 73 and second MR antenna 73 and second MR antenna 73 and fluorescence image processor 58; and the MR image and fluorescence image produced by MR image processor 58 and fluorescence image processor 59 are displayed on monitor 60.

[0060] (Operation) In the fluorescent observation device constituted as in the present embodiment, the subject is place inside a static magnetic field, and endoscope 81 is inserted into the organic cavity of interest. Next, optical probe 71 is inserted inside conduit 82 of endoscope 81.

[0061] Then, the excitation light for fluorescence observation from light source 56 is irradiated onto the organic tissue from light guide 83 of endoscope 81. Due to the irradiation of the organic tissue with the excitation light, auto-fluorescent light is emitted by the organic tissue

[0062] This auto-fluorescent light is imaged by high-sensitivity camera 57 via image guide 72 formed inside optical probe 71, guided into fluorescence image processor 59, and the fluorescence image is displayed on monitor 60.

[0063] Also, by processing the MR signal, obtained by first MR antenna 73 and second MR antenna 73 formed on optical probe 71, at MR image processor 58, a 3-dimensional MR image can similarly be displayed on monitor 60.

[0064] (Effects) This embodiment of the fluorescent observation device, compared to the fourth embodiment, allows the use of an existing endoscope 81 because optical probe 71 is inserted through conduit 82 on endoscope 81 in order to conduct fluorescence observation. Additionally, because it uses optical probe 71, there is great freedom to observe lesions at desired locations. Also, 3-dimensional observations of the organism along its depth are possible because it is equipped with two MR antennae.

[0065] (Sixth Embodiment) Figure 9 to Figure 11 are associated with the sixth embodiment of the present invention. Figure 9 is a schematic diagram showing the constitution of the fluorescent observation device's endoscope with the optical probe inserted through the conduit, Figure 10 is a schematic diagram showing the constitution of the first variation of the endoscope with the optical probe of Figure 9 inserted through the conduit, and Figure 11 is a schematic diagram showing the constitution of the second variation of the endoscope with the optical probe of Figure 9 inserted through the conduit.

[0066] The sixth embodiment is almost identical to the fourth embodiment, so only the differences will be explained, and where the constitution is identical, the same symbols will be used, and explanations will be omitted.

[0067] (Constitution) In the fourth embodiment, the endoscope uses an MR antenna formed inside the tip, but in this embodiment, as shown in Figure 9, the fluorescent observation device includes an endoscope 93, which consists of a first conduit 91 and a second conduit 92; an optical probe 95, which includes an image guide 92 which transmits the fluorescence image from the organic tissue, and is inserted through first conduit 91; and an MR probe 97, which

includes an MR antenna 96, and is inserted through second conduit

[0068] In addition, though not shown, as in the fourth embodiment, the excitation light for fluorescence observation from light source 56 is supplied to a light guide 98 in endoscope 93; the fluorescent light from the organic tissue is transmitted by an image guide 94 in optical probe 95 to high-sensitivity camera 57 where it is imaged, and processed at fluorescence image processor 59; and by processing the MR signal from MR antenna 96 at MR image processor 58, the MR image and fluorescence image generated by MR image processor 58 and fluorescence image processor 59 are displayed on monitor 60.

[0069] (Operation) In the fluorescent observation device constituted as in the present embodiment, the subject is placed inside a static magnetic field, and endoscope 93 is inserted in the targeted organic body cavity. Next, optical probe 95 is inserted inside first conduit 91, and MR probe 97 is inserted inside second conduit 92 of endoscope 93.

[0070] Then, from light guide 98 of endoscope 93, the excitation light for fluorescent observation from light source 56 is irradiated onto the organic tissue. Due to the irradiation of the organic tissue by the excitation light, the organic tissue emits auto-fluorescent light. [0071] This auto-fluorescent light is imaged by high-sensitivity camera 57 via image guide 94 formed inside optical probe 95, guided into fluorescence image processor 59, and displayed on monitor 60 as

a fluorescence image.

[0072] Also, by processing the MR signal, obtained by MR antenna 96 formed in MR probe 97, at MR image processor 68, the MR image is similarly displayed on monitor 60.

[0073] (Effects) In the present embodiment, as in the fourth embodiment, information about the lesion's surface can be observed as a fluorescence image, and also, because information along the depth of the lesion can be observed as an MR image, not only information about the organism's surface, but information along the depth of the organism can be observed, resulting in an increase in diagnostic capabilities.

[0074] Information along the depth can also be observed using an ultrasonic probe instead of MR probe 97.

[0075] Also, the fluorescent observation device can be constituted with an endoscope 102 possessing a large-diameter large conduit 101, as shown in Figure 10, instead of endoscope 93 possessing first conduit 91 and second conduit 92 as shown in Figure 9; and in this case, a semi-circular MR probe 104 with MR antenna 103 inserted through it, and a semicircular optical probe 106 with image guide 105 inserted through it are inserted into large conduit 101. Even with this constitution, operations and effects identical to the present embodiment can be obtained

[0076] Furthermore, operation and effects identical to the present embodiment can be obtained by a fluorescent observation device constituted such that in large conduit 101 in endoscope 102, as shown in Figure 11, a hollow MR probe 111 with built-in MR antenna 103 is inserted, and at the same time, an optical probe 112 with built-in image guide 105 is inserted inside the hollow part of said MR probe 112.

[0077] (Seventh Embodiment) Figure 12 is a schematic diagram showing the fluorescent observation device associated with the seventh embodiment of the present invention.

[0078] (Constitution) The present embodiment is an application of fluorescent observation to surgical treatment, and as shown in Figure 12, in a rigid endoscope 122 possessing a rigid insertion unit 121 which is inserted inside the body cavity via abdominal wall 120, a first conduit connector 124 and a second conduit connector 125 connected to a first conduit and a second conduit (not shown) installed inside insertion unit 121 are installed on grip 123 formed on the end of insertion unit 121, and on ocular unit 126 formed on grip 123, a high-sensitivity camera with built-in image intensifier is connected so that it can be freely connected and removed.

[0079] Then, the present embodiment of fluorescent observation device 130 includes said rigid endoscope 122; a fluorescence image

processor 132 which processes the signal from high-sensitivity camera 127 and displays a fluorescence image on a monitor 131; an excitation light source 133 which is connected to grip 123 and supplies the excitation light to said rigid endoscope 122 in order to conduct fluorescence observation; a surgical instrument controller 136 which controls an ultrasonic disintegration probe 135 which is used to treat lesion 134 and is inserted into the first conduit from first conduit connector 124; and a collection jar 137 which collects the disintegrated tissue using the second conduit via second conduit connector 125.

[0080] (Operation) Insertion unit 121 of rigid endoscope 122 is inserted inside the body cavity via abdominal wall 120. Then, the excitation light for fluorescent observation from excitation light source 133 is irradiated onto the inside of the body cavity via the light guide (not shown) of rigid endoscope 122. When this happens, auto-fluorescent light is emitted by lesion 134 on an organ inside the body cavity, and the auto-fluorescent light is transmitted to the high-sensitivity camera via the image guide (not shown) of rigid endoscope 122. Then, after the image has been processed by fluorescence image processor 132, the fluorescence image of lesion 132 is displayed on monitor 131.

[0081] The operator observes the extent of the infiltration of the lesion using the fluorescence image displayed on monitor 131, and then disintegrates lesion 134 by manipulating ultrasonic disintegration probe 135, which is inserted through the first conduit via first conduit connector 124, and surgical instrument controller 136. The disintegrated legion tissue is collected inside the external collection jar 137 from second conduit connector 125 via the second conduit of rigid endoscope 122.

[0082] (Effects) Thus, in the present embodiment of fluorescent observation device 130, confirmation of the location of lesion 134 inside the abdominal cavity, and confirmation of the extent of infiltration are simplified, so that treatment can be conducted reliably.

[0083] [Additional Remarks]

(Additional Article 1) In relation to fluorescent observation devices for illuminating organic tissue with excitation light to makes observations of said organic tissue by the fluorescent light emitted by said organic tissue, a fluorescent observation device characterized by being equipped with a needle-shaped sheath inserted deep into organic tissue and an ultrasonic observation instrument used to confirm the insertion condition of said needle-shaped sheath in said deep organic tissue, and having an irradiative fiber-optic cable for transmitting said excitation light and an observational fiber-optic cable for transmitting the fluorescent light emitted by said organic tissue formed through the interior of said needle-shaped sheath.

[0084] (Additional Article 2) The fluorescent observation device, as defined in Additional Article 1, characterized by being equipped with a surgical instrument which treats the lesion lying at a depth of said organic tissue with a pharmaceutical which reacts to the irradiation by said excitation light transmitted via said irradiative fiber-optic cable

[0085] (Additional Article 3) The fluorescent observation device as defined in Additional Article 2 with the characteristic that said pharmaceutical is a pharmaceutical prepared for PDT.

[0086] (Additional Article 4) The fluorescent observation device as defined in Additional Article 2 with the characteristic that said pharmaceutical is lumin.

[0087] (Additional Article 5) The fluorescent observation device as defined in Additional Article 2 with the characteristic that said pharmaceutical is TiO₂.

[0088]

[Effects of the Invention] As explained above, the fluorescent observation device of this present invention has the effect of allowing observation of a lesion existing at a depth in an organism by inserting a needle-shaped sheath in tissue existing at a depth of an organism, confirming the insertion condition of the needle-shaped sheath in tissue existing at a depth in an organism using an ultrasonic

observation instrument, and at the same time, transmitting excitation light to the organic tissue using irradiative fiber-optic cable, and transmitting the fluorescent light emitted by said organic tissue using the observational fiber-optic cable.

[Brief explanations of the drawings]

[Figure 1] Schematic diagram showing the constitution of the fluorescent observation device associated with the first embodiment of the present invention.

[Figure 2] Schematic diagram showing the constitution of the convex ultrasonic endoscope used in the fluorescent observation device and passing through the optical probe in Figure 1.

[Figure 3] A drawing showing the monitor which displays the ultrasonic image obtained by the convex ultrasonic endoscope of Figure 2.

[Figure 4] Schematic diagram showing the constitution of the fluorescent observation device associated with the second embodiment of the present invention.

[Figure 5] Schematic diagram showing the constitution of the fluorescent observation device associated with the third embodiment of the present invention.

[Figure 6] Schematic diagram showing the constitution of the fluorescent observation device associated with the fourth embodiment of the present invention.

[Figure 7] Schematic diagram showing the constitution of the optical probe of the fluorescent observation device associated with the fifth embodiment of the present invention.

[Figure 8] Schematic diagram showing the constitution of the endoscope with the optical probe of Figure 7 inserted through the conduit.

[Figure 9] Schematic diagram regarding the fifth embodiment of the present invention showing the constitution of the fluorescent observation device's endoscope with the optical probe inserted through the conduit.

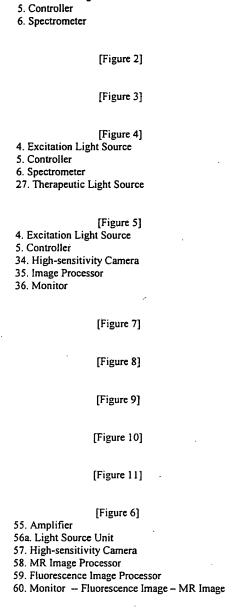
[Figure 10] Schematic diagram showing the constitution of the first variation of the endoscope with the optical probe of Figure 9 inserted through the conduit.

[Figure 11] Schematic diagram showing the constitution of the second variation of the endoscope with the optical probe of Figure 9 inserted through the conduit.

[Figure 12] Schematic diagram showing the constitution of the fluorescent observation device associated with the seventh embodiment of the present invention.

[Explanation of Symbols]

- 1 ··· Fluorescent observation device
- 2 ··· Sheath
- 3 ··· Optical probe
- 4 ··· Excitation light source
- 5 ··· Controller
- 6 ··· Spectrometer
- 7 ··· First conduit
- 8 ··· Second conduit
- 9 ··· First fiber-optic cable
- 10 ··· Second fiber-optic cable
- 11 ··· Tip
- 12 ··· Organic tissue
- 13 ··· Objective optic module
- 14 ··· Ultrasonic receiver
- 15 ··· Convex ultrasonic endoscope
- 16 ··· Conduit
- 17 ··· External monitor



[Figure 12]

132. Fluorescence Image Processor 133. Excitation Light Source 136. Surgical Instrument controller

131. Monitor

[Figure 1]

4. Excitation Light Source

Continued from Front Page

Hitoshi UENO (72) Inventor

at Olympus Optical Co. Ltd. 2-43-2 Hatagaya, Shibuya-ku, Tokyo

(72) Inventor

Sakae TAKEHATA at Olympus Optical Co. Ltd. 2-43-2 Hatagaya, Shibuya-ku, Tokyo



MACHINE-ASSISTED TRANSLATION (MAT):

(19)【発行国】

(19)[ISSUING COUNTRY]

日本国特許庁(JP)

Japanese Patent Office (JP)

(12)【公報種別】

公開特許公報(A)

Laid-open (kokai) patent application number (A)

(11)【公開番号】

(11)[UNEXAMINED PATENT NUMBER]

特開平11-155812

Provisional Publication No. 11-155812

(43)【公開日】

(43)[DATE OF FIRST PUBLICATION]

平成11年(1999)6月1

5日

June 15th, Heisei 11 (1999)

(54)【発明の名称】

(54)[TITLE]

蛍光観察装置

Fluorescent observation apparatus

(51)【国際特許分類第6版】

A61B 1/06

(51)[IPC]

A61B 1/06

1/00 300 1/00 300

[FI]

A61B 1/06

[FI]

В

A61B 1/06

В

1/00 300 F 1/00

300 F

【審査請求】

[EXAMINATION REQUEST]

未請求

UNREQUESTED

【請求項の数】 1 [NUMBER OF CLAIMS] One.

【出願形態】 OL

[Application form] OL

【全頁数】 9

[NUMBER OF PAGES] Nine



(21)【出願番号】

(21)[APPLICATION NUMBER]

特願平9-331991

Unexamined Japanese patent 9-331991

(22)【出願日】

(22)[DATE OF FILING]

平成9年(1997) 12月2 December 2nd, Heisei 9 (1997)

日

(71)【出願人】

(71)[PATENTEE/ASSIGNEE]

【識別番号】

[PATENTEE/ASSIGNEE CODE]

000000376

000000376

【氏名又は名称】

オリンバス光学工業株式会社

Olympus Optical Co., Ltd. K.K.

【住所又は居所】

[ADDRESS]

東京都渋谷区幡ヶ谷2丁目43

番2号

(72)【発明者】

(72)[INVENTOR]

【氏名】 平尾 勇実 Hirao, Isami

【住所又は居所】

[ADDRESS]

東京都渋谷区幅ケ谷2丁目43

番2号 オリンバス光学工業株

式会社内

(72)【発明者】

(72)[INVENTOR]

【氏名】 道口 信行

Michiguchi, Nobuyuki

【住所又は居所】

[ADDRESS]



東京都渋谷区幅ヶ谷2丁目43 番2号 オリンパス光学工業株 式会社内

(72)【発明者】

(72)[INVENTOR]

【氏名】 金子 守

Kaneko, Mamoru

【住所又は居所】

[ADDRESS]

東京都渋谷区幡ヶ谷2丁目43 番2号 オリンパス光学工業株 式会社内

(72)【発明者】

(72)[INVENTOR]

【氏名】 上野 仁士

Ueno, Hitoshi

【住所又は居所】

[ADDRESS]

東京都渋谷区幡ヶ谷2丁目43 番2号 オリンパス光学工業株 式会社内

(72)【発明者】

(72)[INVENTOR]

【氏名】 竹端 栄

Takehata, Sakae

【住所又は居所】

[ADDRESS]

東京都渋谷区幅ヶ谷2丁目43 番2号 オリンパス光学工業株 式会社内

(74)【代理人】

(74)[PATENT ATTORNEY]



【弁理士】

【氏名又は名称】 伊藤 進

Ito, Susumu

(57)【要約】

(57)[SUMMARY]

【課題】

生体の深部に存在する病変部の 観察を行う

【解决手段】

蛍光観察装置1は、生体へ穿刺 する先端部のみ硬性で他は可撓 性を有する針状のシース2から 成る光ブローブ3と、蛍光観察 を行うための励起光を光ブロー ブ3に供給する励起用光源4 と、励起用光源4からの励起光 の光プローブ3への供給を制御 する制御装置5と、光ブローブ 3からの励起光による生体深部 の病変部からの自家蛍光により 組織を診断するスペクトロメー 夕6とを備えて構成される。光 プローブ3の針状のシース2の 内部には、第1チャンネル7及 び第2チャンネル8が設けら れ、第1チャンネルフには生体 深部の病変部からの自家蛍光を スペクトロメータ6に伝送する 第1の光ファイバタが、また第 2チャンネル8には励起用光源 4からの励起光を伝送する第2

[SUBJECT]

To observe the disease part which exists in the deep part of the organism.

[SOLUTION]

The fluorescent observation apparatus 1, the optical probe 3 with which only the end which transfixes to the organism is hard and needle-like, and the sheath 2 having flexibility, the light source for excitation 4 which supplies the excitation light for performing fluorescent observation to the optical probe 3, the control apparatus 5 which controls supply to the optical probe 3 of the excitation light from the light source for excitation 4, the spectrometer 6 which diagnoses a tissue according to the self-fluorescence from the disease part of the organism deep part by the excitation light from the optical probe 3.

It has these and it is constituted.

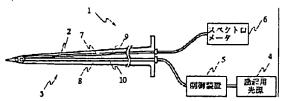
The 1st 7 and second channel 8 are provided on the inside of the needle-like sheath 2 of the optical probe 3.

In the 1st channel 7, the first optical fibre 9 which transmits the self-fluorescence from the disease part of the organism deep part to a spectrometer 6, Moreover the 2nd optical fibre



設されている。

の光ファイバ 1 Oがそれぞれ配 10 which transmits the excitation light from the light source for excitation 4 in the second channel 8 is respectively arranged.



[translation of Japanese text in Selection Diagram] refer to EXPLANATION OF DRAWINGS

【特許請求の範囲】

[CLAIMS]

【請求項1】

生体組織に励起光を照射し、前 記生体組織から発生する蛍光に 光観察装置において、

生体深部組織に穿刺する針状シ ースと、

前記針状シースの前記生体深部 組織への穿刺状態を確認する超 音波観察手段とを備え、

前記針状シースの内部に前記励 起光を伝送する照明用光ファイ バと、前記生体組織から発生す る蛍光を伝送する観察用光ファ る蛍光観察装置。

[CLAIM 1]

Excitation light is irradiated to an organism tissue.

より前記生体組織を観察する蛍 In the fluorescent observation apparatus which observes the above-mentioned organism tissue according to the fluorescence generated from the above-mentioned organism tissue, the needle-like sheath which transfixes to an organism deep-part tissue, and ultrasonic observation means to confirm the transfixed state to the above-mentioned organism deeppart tissue by the above-mentioned needle-like sheath. It has these.

The optical fibre for illumination which イバとを設けたことを特徴とす transmits above-mentioned excitation light inside the above-mentioned needle-like sheath, and the optical fibre for observation which transmits the fluorescence generated from the above-mentioned organism tissue were provided.



fluorescent observation apparatus characterized by the above-mentioned.

【発明の詳細な説明】

[DETAILED DESCRIPTION OF INVENTION]

[0001]

[0001]

【発明の属する技術分野】

本発明は被検査対象に励起光を 照射し被検査対象から発する蛍 光より疾患部位を観察する蛍光 観察装置、更に詳し<は被検査 対象への励起光の照射部分に特 徴のある蛍光観察装置に関す る。

[0002]

[TECHNICAL FIELD]

This invention is fluorescent observation apparatus which observes an illness site from the fluorescence which excitation light is irradiated for a tested object and emitted from a tested object. Furthermore in detail, it is related with the fluorescent observation apparatus which has the characteristic in the irradiation part of the excitation light to a tested object.

[0002]

【従来の技術】

へ励起光を照射し、この励起光 によって生体組織から直接発生 する自家蛍光や生体へ注入して おいた薬物の蛍光を2次元画像 として検出し、その蛍光像から 生体組織の変性や癌等の疾患状 態(例えば、疾患の種類や浸潤 **範囲)を診断する技術が用いら** れつつあり、例えば特開平8-252218号公報に示される ように、この蛍光観察を行うた fluorescent image is used. めの蛍光観察装置が種々提案さ

[PRIOR ART]

近年、生体組織の観察対象部位 In recent years, excitation light is irradiated to the site for observation of an organism tissue. It detects the fluorescence of the medicine injected into the organism and the selffluorescence directly generated from an organism tissue by this excitation light as a twodimensional image.

> The technique that illness states (for example, the kind and permeation extent of the illness), such as the modified of an organism tissue and cancer, are diagnosed from the

For example, as shown in the Provisional-



れている。

Publication-No. 8-252218 gazette, the various proposal of the fluorescent observation apparatus for performing this fluorescent observation is carried out.

[0003]

自家蛍光においては、生体組織 に励起光を照射すると、その励 起光より長い波長の蛍光が発生 する。生体における蛍光物質と しては、例えばコラーゲン、N ADH (ニコチンアミドアデニ ンヌクレオチド)、FMN(フ ラヒンモノヌクレオチト), ヒ リジンヌクレオチド等がある。 最近では、このような蛍光を発 生する生体内因物質と疾患との 相互関係が明確になりつつあ り、これらの蛍光により癌等の 診断が可能である。

[0004]

また、薬物の蛍光においては、 生体内へ注入する蛍光物質とし ては、HpD(ヘマトポルフィ リン), Photofrin, ALA(δ —amino levulinic acid) 等が用 いられる。これらの薬物は癌な どへの集積性があり、これを生 property, such as towards cancer. 体内に注入して蛍光を観察する ことで疾患部位を診断できる。 また、モノクローナル抗体に蛍 光物質を付加させ、抗原抗体反 応により病変部に蛍光物質を集 **積させる方法もある。**

[0003]

For self-fluorescence, if excitation light is irradiated to an organism tissue, fluorescence of a wavelength longer than the excitation light will occur.

It uses as the fluorescent material in the organism, for example, there are a collagen, NADH (nicotinamide adenine nucleotide) and **FMN** (flavin mononucleotide), ?biridine? nucleotide, etc.

Recently, the interactive relationship of ?factor-substance? in the living body and the illness which generate such a fluorescence is becoming clear, and the diagnosis of cancer etc. is possible by these fluorescence.

[0004]

Moreover, in the fluorescence of a medicine, HpD (hematoporphyrin), Photofrin, ALA((delta)amino levulinic acid), etc. are used as a fluorescent material injected into the living body.

These medicines have accumulation

An illness site can be diagnosed by injecting this in the living body and observing fluorescence.

Moreover, a fluorescent material is added to a monoclonal antibody, and there is also a method of making a disease part accumulate a fluorescent material by an antigen antibody



reaction.

[0005]

励起光としては例えばレーザ 光、水銀ランプ、メタルハライ トランプ等が用いられ、励起光 を生体組織へ照射することによ って観察対象部位の蛍光像を得 る。この励起光による生体組織 における微弱な蛍光を検出して 2次元の蛍光画像を生成し、観 察、診断を行う。

[0006]

[0005]

It uses as excitation light, for example, a laser light, a mercury lamp, a metal halide lamp, etc. are used.

The fluorescent image of the site for observation is obtained by irradiating excitation light to an organism tissue, the slight fluorescence in the organism tissue by this excitation light is detected, and a twodimensional fluorescent image is formed, and an observation and a diagnosis are performed.

[0006]

【発明が解決しようとする課 [PROBLEM ADDRESSED]

題】

しかしながら、特開平8-25 来の蛍光観察装置においては、 生体の表面組織に励起光を照射 tissue of the organism. し、生体の表面組織から発する ているだめ、生体の表面に存在 する病変部しか観察できず、生 体の深部に存在する病変を観察 できないという問題がある。

[0007]

本発明は、上記事情に鑑みてな されたものであり、生体の深部 に存在する病変部を観察するこ

However, in the conventional fluorescent observation apparatus shown in the 2218号公報等に示される従 Provisional-Publication-No. 8-252218 gazette etc., excitation light is irradiated to the surface

Since the self-fluorescence emitted from the 自家蛍光を経内視鏡的に観察し surface tissue of the organism is observed perendoscopically, there is a problem that only the disease part which exists on the surface of the organism can be observed, and the disease which exists in the deep part of the organism cannot be observed.

[0007]

This invention is made in view of the abovementioned situation.

It aims at providing the fluorescent とのできる蛍光観察装置を提供 observation apparatus which can be observed



することを目的としている。

the disease part which exists in the deep part of the organism.

[0008]

[8000]

[SOLUTION OF THE INVENTION]

The fluorescent observation apparatus of this invention irradiates excitation light to an organism tissue.

In the fluorescent observation apparatus which observes the above-mentioned organism tissue according to the fluorescence generated from the above-mentioned organism tissue, it has the needle-like sheath which transfixes to an organism deep-part tissue, and ultrasonic observation means to confirm the transfixed state to the above-mentioned organism deep-part tissue of the above-mentioned needle-like sheath.

The optical fibre for illumination which transmits above-mentioned excitation light inside the above-mentioned needle-like sheath, and the optical fibre for observation which transmits the fluorescence generated from the above-mentioned organism tissue are provided.

[0009]

本発明の蛍光観察装置では、前 In the fluorescent 記針状シースを前記生体深部組 invention, the a 織に穿刺し、前記超音波観察手 sheath is transfix 段により前記針状シースの前記 organism deep-pa 生体深部組織への穿刺状態を確 While confirming 認すると共に、前記照明用光フ above-mentioned アイバにより前記生体組織に前 the above-mentioned 記励起光を伝送し、前記観察用 above-mentioned

[0009]

In the fluorescent observation apparatus of this invention, the above-mentioned needle-like sheath is transfixed to the above-mentioned organism deep-part tissue.

While confirming the transfix state to the above-mentioned organism deep-part tissue of the above-mentioned needle-like sheath by the above-mentioned ultrasonic observation



から発生する蛍光を伝送するこ とで、生体の深部に存在する病 変部の観察を行うことを可能と する。

光ファイバにより前記生体組織 means, above-mentioned excitation light is transmitted to the above-mentioned organism tissue by the above-mentioned optical fibre for illumination.

> It is enabled to observe the disease part which exists in the deep part of the organism, by transmitting the fluorescence generated from the above-mentioned organism tissue by the above-mentioned optical fibre for observation.

[0010]

[0010]

【発明の実施の形態】

る。

[Embodiment]

以下、図面を参照しながら本発 Hereafter, the embodiment of this invention is 明の実施の形態について述べ described, referring to drawings.

[0011]

(第1の実施の形態)図1ない し図3は本発明の第1の実施の 形態に係わり、図1は蛍光観察 装置の構成を示す構成図、図2 は図1の光プローブを挿通する 蛍光観察装置に用いられるコン ベックス型超音波内視鏡の構成 を示す構成図、図3は図2のコ ンベックス型超音波内視鏡によ り得られた超音波画像を表示す るモニタを示す図である。

[0011]

(First embodiment) Fig. 1 or 3 concerns the first embodiment of this invention.

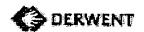
Diagram 1 is a block diagram showing the fluorescent composition of observation apparatus. diagram 2 is a block diagram showing the composition of the convex type ultrasound endoscopy used for the fluorescent observation apparatus which passes through the optical probe in the diagram 1. diagram 3 is a diagram showing the monitor which displays the ultrasonic image obtained by the convex type ultrasound endoscopy in the diagram 2.

[0012]

(構成) 図1に示すように、本 (Composition) 実施の形態の蛍光観察装置1

[0012]

As shown in diagram 1, the fluorescent は、生体へ穿刺する先端部のみ observation apparatus 1 of this embodiment is,



硬性で他は可撓性を有する針状 のシース2から成る光プローブ 3と、蛍光観察を行うための励 起光を光プローブ3に供給する 励起用光源4と、励起用光源4 からの励起光の光プローブ3へ の供給を制御する制御装置5 と、光プローブ3からの励起光 による生体深部の病変部からの 自家蛍光により組織を診断する スペクトロメータ6とを備えて 構成される。

the optical probe 3 with which only the end which transfixes to the organism is hard, and the needle-like sheath 2 having flexibility, the light source for excitation 4 which supplies the excitation light for performing fluorescent observation to the optical probe 3, the control apparatus 5 which controls supply to the optical probe 3 of the excitation light from the light source for excitation 4, and the spectrometer 6 which diagnoses a tissue according to the selffluorescence from the disease part of the organism deep part by the excitation light from the optical probe 3.

It has these and it is constituted.

[0013]

光プローブ3の針状のシース2 の内部には、第1チャンネル7 及び第2チャンネル8が設けら れ、第1チャンネル7にはスペ クトロメータ6に接続され生体 深部の病変部からの自家蛍光を スペクトロメータ6に伝送する 第1の光ファイバタが、また第 2チャンネル8には励起用光源 4に揺続され励起用光源4から の励起光を伝送する第2の光フ アイバー〇がそれぞれ配設され ている。

[0014]

うに、先端部11に設けられた 体腔内の生体組織12を光学観

[0013]

inside the needle-like sheath 2 of the optical probe 3, the 1st channel 7 and the second channel 8 are provided.

The first optical fibre 9 which is connected to the 1st channel 7 at a spectrometer 6, and transmits the self-fluorescence from the disease part of the organism deep part to a spectrometer 6, moreover the 2nd optical fibre 10 which is connected to the light source for excitation 4 in the second channel 8, and transmits the excitation light from the light source for excitation 4 are respectively arranged.

[0014]

光プローフ3は、図2に示すよ The optical probe 3 should be shown in a diagram 2. In relation to the object optical system 13 which observes optically the 察する対物光学系 1 3 に対して organism tissue 12 intra-corporeal provided on 挿入方向前方に超音波振動子を the end 11, into the channel 16 of the convex



円弧状の凸状に配置した超音波 送受信部 1 4を有するコンペッ クス型超音波内視鏡 15のチャ ンネル16内に插通されて用い られ、蛍光観察装置1において は、コンベックス型超音波内視 鏡15は、図示はしないが、観 察用照明光を供給する観察用光 源及び超音波送受信部14亿よ り超音波を送受し超音波画像を 生成する超音波観測装置に揺続 され、例えば体腔内の生体組織 12の光学像を接眼部で観察し ながら超音波観測装置からの超 音波画像を、図3に示すような 外部モニタ17に表示すること で、光プローブ3の生体組織1 2への穿刺状態を確認可能な構 成となっている。

type ultrasound endoscopy 15 which has an ultrasonic vibrator the circular ultrasonic transmitting-and-receiving part 14 configured convex-shaped in the insertion direction passes through and it is used.

In the fluorescent observation apparatus 1, the convex type ultrasound endoscopy 15 is not illustrated.

However, it connects with the ultrasonic observation apparatus which sends and receives an ultrasonic wave by the light source for observation and the ultrasonic transmittingand-receiving part 14 which supply the illumination light for observation, and forms an ultrasonic image.

For example, by displaying on the external monitor 17 which shows the ultrasonic image from an ultrasonic observation apparatus in a diagram 3, observing the optical image of the organism tissue 12 intra-corporeal in an eyepiece part, it is the composition which can confirm the transfix state to the organism tissue 12 of the optical probe 3.

[0015]

(作用) 次に、このように構成 された本実施の形態の蛍光観察 装置1の作用について説明す る。

[0015]

(Effect)

Next, an effect of the fluorescent observation apparatus 1 of this embodiment constituted in this way is demonstrated.

[0016]

蛍光観察装置1の光プローブ3 鏡15のチャンネル16を介し て生体組織 12に穿刺される。

[0016]

The transfix of the optical probe 3 of the は、コンペックス型超音波内視 fluorescent observation apparatus 1 is carried out to the organism tissue 12 via the channel 16 of the convex type ultrasound endoscopy 15. この時、コンペックス型超音波 At this time, the ultrasonic image of the deep



内視鏡 15 に接続された外部モニタ 17 には、生体組織 12の深部の超音波画像が表示され、 術者は生体組織 12の深部の病変部 18 (図3参照)に確実に 光プローブ3が穿刺していることを確認しながら、光プローブ 3を誘導する。

[0017]

そして、術者は生体組織12の深部の目的とする病変部18に光フローブ3が確実に穿刺したことを確認したら、外部に設けた制御装置5を操作し、励起用光源4から病変部18に励起光を供給し、この励起光は、第2の光ファイバ10を介して生体組織12の深部の病変部18に照射される。

[0018]

励起光が照射されると、生体組 Irradiation 織12の深部の病変部18から fluorescer は自家蛍光が放射され、自家蛍 deep part 光は第1の光ファイバタを介し fluorescer て外部に設けられたスペクトロ externally メータ6に導かれる。そして、 And, an 術者はスペクトロメータ6を読 and perfo み取ることで、生体組織12の disease pa 深部の病変部18の蛍光観察を tissue 12. 行う。

[0019]

(効果) このように本実施の形態の蛍光観察装置1では、生体

part of the organism tissue 12 is displayed on the external monitor 17 connected to the convex type ultrasound endoscopy 15.

An operator guides the optical probe 3, confirming that the optical probe 3 is carrying out the transfix to the disease part 18 (diagram 3 reference) of the deep part of the organism tissue 12 reliably.

[0017]

And, if the operator checks that the optical probe 3 has transfixed reliably to the disease part 18 objective of the deep part of the organism tissue 12, the control apparatus 5 provided externally will be operated.

Excitation light is supplied to the disease part 18 from the light source for excitation 4.

の光ファイバ 1 Oを介して生体 These excitation light is irradiated by the 組織 1 2 の深部の病変部 1 8 に disease part 18 of the deep part of the organism 照射される。 tissue 12 via the 2nd optical fibre 10.

[0018]

Irradiation of excitation light radiates a selffluorescence from the disease part 18 of the deep part of the organism tissue 12, and a selffluorescence is guided to the spectrometer 6 externally provided via the first optical fibre 9.

And, an operator is reading a spectrometer 6 and performs fluorescent observation of the disease part 18 of the deep part of the organism tissue 12.

[0019]

(Effect)

Not only for the surface part of the organism



組織12の深部の病変部18に 針状の光プローブ3を穿刺する ことで、生体組織12の表面部 のみならず、生体組織12の深 部の病変部18の蛍光観察が可 能となる。また、光ブローブ3 の生体組織12の深部への穿刺 状態をコンペックス型超音波内 視鏡15で観察しているため、 術者は確実に病変部18へ穿刺 することができる。

[0020]

なお、本実施の形態では、コンベックス型超音波内視鏡 15により、光ブローブ3の穿刺状態を確認しているが、これに限らず、ラシアル型あるいはリニア型の超音波内視鏡で光ブローブ3の穿刺状態の確認を行い、生体組織 12の深部の病変部 18の蛍光観察するようにしてもよい。

[0021]

(第2の実施の形態)図4は本発明の第2の実施の形態に係る 蛍光観察装置の構成を示す構成 図である。

[0022]

第2の実施の形態は、第1の実施の形態とほとんど同じであるので、異なる点のみ説明し、同一の構成には同じ符号をつけ説

tissue 12 in transfixing the needle-like optical probe 3 to the disease part 18 of the deep part of the organism tissue 12 with the fluorescent observation apparatus 1 of this embodiment in this way, also the fluorescent observation of the disease part 18 of the deep part of the organism tissue 12 can be performed.

Moreover, since the transfix state to the deep part of the organism tissue 12 of the optical probe 3 is observed by the convex type ultrasound endoscopy 15, an operator can reliably transfix to the disease part 18.

[0020]

In addition, in this embodiment, the transfix state of the optical probe 3 is confirmed by the convex type ultrasound endoscopy 15.

However, it does not restrict to this, and the transfix state of the optical probe 3 is confirmed by a radial type or a linear type of ultrasound endoscopy.

The disease part 18 of the deep part of the organism tissue 12 may be observed fluorescently.

[0021]

(2nd embodiment) diagram 4 is a block diagram showing the composition of the fluorescent observation apparatus based on the 2nd embodiment of this invention.

[0022]

Since the 2nd embodiment is almost the same as that of a first embodiment, it demonstrates only the different items.

The same code for identical composition is



明は省略する。

[0023]

(構成) 図4に示すように、本 実施の形態の蛍光観察装置1a においては、光ブローブ3の針 状シース2の内部に、第1チャ ンネルフ及び第2チャンネル8 の他に第3チャンネル21が設 けられ、この第3チャンネル2 1は蛍光診断を行うための薬剤 22及び治療用の薬剤23が注 入可能に外部に設けたシリンジ 24、25に揺続されており、 バルブ26を制御することによ り、各々を選択的に第3チャン っている。

[0024]

また、本実施の形態の蛍光観察 装置1aは、治療用光源27を 備えており、制御装置5により 第2チャンネル8に設けられた **源27からの光を選択して照** 射・供給することができるよう になっている。

[0025]

なお、蛍光診断用の薬剤22と しては、例えばヘマトボルフィ リン(HPD)等が用いられ、 治療用の薬剤23としては、ル ミン等が用いられる。

attached and description is omitted.

[0023]

(Composition)

As shown in a diagram 4, in fluorescent observation apparatus 1a of this embodiment, the 1st channel 7 and the 3rd channel 21 other than the second channel 8 are provided on the inside of the needle-like sheath 2 of the optical probe 3.

As for this 3rd channel 21, the chemical agent 22 for performing fluorescent diagnosis and the chemical agent 23 for treatments are in the syringes 24 and 25 connected externally for possible injection.

By controlling a valve 26, each can be ネル21 に供給できるようにな selectively supplied now to the 3rd channel 21.

[0024]

Moreover, fluorescent observation apparatus 1a of this embodiment has the light source for treatments 27.

The excitation light from the light source for 第2の光ファイバ 1 Oに励起用 excitation 4 and the light from the light source 光源4からの励起光と治療用光 for treatments 27 are chosen as the 2nd optical fibre 10 provided on the second channel 8 with the control apparatus 5, it can irradiate or supply now.

[0025]

In addition, it is considered as the chemical agent 22 for fluorescent diagnosis, for example, hematoporphyrin (HPD) etc. is used.

?lumine? etc. is used as a chemical agent 23 for treatments.



[0026]

その他の構成は第1の実施の形 態と同じである。

[0027]

(作用) このように構成された 本実施の形態の蛍光観察装置 1 aの光プローブ3は、第1実施 の形態と同じく、コンベックス 型超音波内視鏡 15のチャンネ ル16を介して生体組織12の 深部に挿入される(図2参照)。 そして、コンベックス型超音波 reference). 内視鏡15からの超音波画像を 外部モニタイプにより観察しな がら生体組織 12の深部の病変 部18へ光プローブ3が誘導さ れる。

[0028]

術者が生体組織12の深部の病 変部18に光ブローブ3が穿刺 されたことを確認すると、バル ブ26を制御し、シリンシ24 から蛍光診断用の薬剤22を第 3チャンネル21を介して病変 部18に注入する。次に、制御 装置5により診断用の励起用光 源4から診断用の励起光を第2 の光ファイバ10を介して生体 組織12の深部の病変部18に 照射する。

[0029]

[0026]

Other composition is the same as that of the first embodiment.

[0027]

(Effect)

Thus the optical probe 3 of fluorescent observation apparatus 1a of this constituted embodiment is similarly inserted in the deep part of the organism tissue 12 via the channel 16 of the convex type ultrasound endoscopy 15. as in the 1st embodiment (diagram 2

And, the optical probe 3 is guided to the disease part 18 of the deep part of the organism tissue 12, observing the ultrasonic image from the convex type ultrasound endoscopy 15 with the external monitor 17.

[0028]

An operator's confirmation of that the optical probe 3 transfixed the disease part 18 of the deep part of the organism tissue 12 controls a valve 26.

The chemical agent 22 for fluorescent diagnosis is injected into the disease part 18 via the 3rd channel 21 from a syringe 24...

Next, the excitation light for a diagnosis are irradiated among the disease part 18 of the deep part of the organism tissue 12 via the 2nd optical fibre 10 from the light source for excitation 4 for a diagnosis with a control apparatus 5.

[0029]



すると、蛍光診断用の薬剤22 が病変部18に注入されている **ため、病変部 1 8 からは蛍光が** 放射される。この蛍光は第1チ ヤンネルフに設けられた第1の 光ファイバタを介して外部に設 けられたスペクトロメータ6に 導かれる。そして、術者がスペ クトロメータ6を観察すること で、病変部18の蛍光診断が可 能となる。

Then, since the chemical agent 22 for fluorescent diagnosis is injected into the disease part 18, a fluorescence is radiated from the disease part 18.

This fluorescence is guided spectrometer 6 externally provided via the first optical fibre 9 provided on the 1st channel 7.

And, fluorescent diagnosis of the disease part 18 is made by an operator observing a spectrometer 6.

[0030]

生体組織 12の深部の病変部 1 8の観察が終わった後、次に、 外部に設けられたシリンジ25 から治療用の薬剤23を第3チ ヤンネル21を介して生体組織 12の深部の病変部18に注入 する。そして、外部に設けられ た治療用光源27から治療用の 光を制御装置5を介して第2の 光ファイバ10へ導く。

[0030]

After an observation of the disease part 18 of the deep part of the organism tissue 12 finishes, next, the chemical agent 23 for treatments is injected into the disease part 18 of the deep part of the organism tissue 12 via the 3rd channel 21 from the syringe 25 provided externally.

And, the light for treatments is guided to the 2nd optical fibre 10 via a control apparatus 5 from the light source for treatments 27 provided externally.

[0031]

すると、光プローブ3からは治 療用の光が放射され、治療用薬 体組織12の深部の病変部18 の治療が行われる。

[0031]

Then, the light for treatments is radiated from the optical probe 3, the chemical agent for 剤23と化学反応を起こし、生 treatments 23 undergoes chemical reaction, and the treatment of the disease part 18 of the deep part of the organism tissue 12 is performed.

[0032]

(効果) このように本実施の形 態の蛍光観察装置1aでは、第

[0032]

(Effect)

Thus in addition to the effect of a first



1の実施の形態の効果に加え、 生体組織12の深部の病変部1 8治療も可能となる。

embodiment. fluorescent observation in apparatus 1a of this embodiment, disease part 18 treatment of the deep part of the organism tissue 12 is also made.

[0033]

(第3の実施の形態) 図5は本 発明の第3の実施の形態に係る 図である。

[0034]

第3の実施の形態は、第1の実 施の形態とほとんど同じである ので、異なる点のみ説明し、同 ーの構成には同じ符号をつけ説 identical 明は省略する。

[0035]

(構成) 図5に示すように、本 実施の形態の蛍光観察装置1b においては、光プローブ3の針 状シース2の内部に、第1チャ ンネル7及び第2チャンネル8 の他に第3チャンネル31が設 けられ、この第3チャンネル3 1は治療用の薬剤32が注入可 能に外部に設けたシリンシ33 に推続されている。

[0036]

また、本実施の形態の蛍光観察 装置1bでは、第1チャンネル 7に設けられた第1の光ファイ

[0033]

(Third embodiment) diagram 5 is a block diagram showing the composition of the 蛍光観察装置の構成を示す構成 fluorescent observation apparatus based on the third embodiment of this invention.

[0034]

Since the third embodiment is almost the same as that of the first embodiment, it demonstrates only the different items, and the same code for composition is attached description is omitted.

[0035].

(Composition)

As shown in a diagram 5, in fluorescent observation apparatus 1b of this embodiment, the 1st channel 7 and the 3rd channel 31 other than the second channel 8 are provided on the inside of the needle-like sheath 2 of the optical probe 3.

This 3rd channel 31 is connected to the syringe 33 which provided the chemical agent 32 for treatments connected externally for possible injection.

[0036]

Moreover, the self-fluorescence from the disease part 18 of the deep part of the organism tissue 12 which transmitted the first optical fibre バタを伝送した生体組織 1 2の 9 provided on the 1st channel 7 in fluorescent



深部の病変部18からの自家蛍 光は、イメージインテンシファ イヤを内蔵する高感度カメラ3 4で撮像され、画像処理装置3 5により信号処理され、モニタ 36にて術者が病変部18の蛍 光画像を観察可能な構成となっ ている。

recorded with the high-sensitivity camera 34 which contains an image intensifier, signal processing is carried out by the image processing device 35, and with a monitor 36, it is the composition whereby the fluorescent image of the disease part 18 can be observed by the operator.

observation apparatus 1b of this embodiment is

[0037]

ここで、制御装置5により供給 が制御される励起用光源4は、 例えばヘリウム、カドミウムレ ーザが用いられ、励起光の波長 は442nmである。また、治 療用の薬剤32としては、酸化 る。

[0037]

Here, as for the light source for excitation 4 with which supply is controlled by the control apparatus 5, helium and a cadmium laser are used, for example, and the wavelength of excitation light is 442 nm.

Moreover, titanium-oxide (TiO2) is used as a チタン(TiO2)が用いられ chemical agent 32 for treatments.

[0038]

その他の構成は第1の実施の形 態と同じである。

[0038]

Other composition is the same as that of the first embodiment.

[0039]

(作用) このように構成された 本実施の形態の蛍光観察装置 1 bの光プローブ3は、第1実施 の形態と同じく、コンベックス 型超音波内視鏡 15のチャンネ ル16を介して生体組織12の 深部に挿入される(図2参照)。 そして、コンベックス型超音波 内視鏡 15からの超音波画像を 外部モニタ17により観察しな がら生体組織 12の深部の病変 部 18へ光プローブ 3 が誘導さ the external monitor 17.

[0039]

(Effect)

Thus the optical probe 3 of fluorescent observation apparatus 1b of this constituted embodiment is similarly inserted in the deep part of the organism tissue 12 via the channel 16 of the convex type ultrasound endoscopy 15 with the 1st embodiment (diagram 2 reference).

And, the optical probe 3 is guided to the disease part 18 of the deep part of the organism tissue 12, observing the ultrasonic image from the convex type ultrasound endoscopy 15 with



れる。

[0040]

そして、術者は外部モニタ17 で光プロープ3の生体組織12 の深部の病変部18への穿刺を確認し、生体組織12の深部の 病変部18へ穿刺したことが確 認できたら、外部に設けられた 励起用光源4から442nmの 蛍光観察用の励起光を供給す る。

[0041]

この励起光は、第2の光ファイバ10を介して生体組織12の深部の病変部18に照射される。442nmの励起光が照射されると、生体組織12の深部からは自家蛍光が放射される。この自家蛍光は第1の光ファイバ9を介して外部に設けられた高度度カメラ34で捉えられ、画像処理装置35で処理され、外部に設けられたモニタ36に病変部18が蛍光画像として表示される。

[0042]

術者はモニタ36で病変部18 が確認できたら、次に外部に設けられた治療用の薬剤32としての酸化チタン(TiO2)を 第3チャンネル31を介して生体組織12の深部の病変部18 に注入を行う。そして、外部に

[0040]

And, an operator confirms the transfix to the disease part 18 of the deep part of the organism tissue 12 of the optical probe 3 with the external monitor 17.

If it is verified having transfixed to the disease part 18 of the deep part of the organism tissue 12, the 442 nm excitation light for fluorescent observation will be supplied from the light source for excitation 4 provided externally.

[0041]

These excitation light is irradiated by the disease part 18 of the deep part of the organism tissue 12 via the 2nd optical fibre 10.

If 442 nm excitation light is irradiated, a selffluorescence is radiated from the deep part of the organism tissue 12.

This self-fluorescence is caught with the highsensitivity camera 34 externally provided via the first optical fibre 9, it is processed by the image processing device 35, and the disease part 18 is displayed as a fluorescent image by the monitor 36 provided externally.

[0042]

An operator will inject titanium-oxide (TiO2) as a chemical agent 32 for treatments next, provided externally, into the disease part 18 of the deep part of the organism tissue 12 via the 3rd channel 31, if the disease part 18 can be confirmed with a monitor 36.

And, a 442 nm light is irradiated to the



設けられたヘリウム、カドミウムレーザからなる励起用光源4から442nmの光を第2の光ファイバ10を介して生体組織12の深部の病変部18に照射する。生体組織12の深部には治療用薬剤36の酸化チタン(TiO2)が注入されているため、励起光源4から放射された42nmの光と酸化還元反応を起こし、生体組織12の深部の病変部18は治療されることなる。

[0043]

(効果) このように本実施の形態の蛍光観察装置1bでは、第2の実施の形態と同様に、第1の実施の形態の効果に加え、生体組織12の深部の病変部18治療も可能となる。また、第2の実施の形態と比べ、治療用光源が1つの光源で共用でき、システムの小型化が図れる。さらに、生体組織12の深部の情報を画像として表示しているため、診断能が向上する。

[0044]

(第4の実施の形態)図6は本発明の第4の実施の形態に係る 蛍光観察装置の構成を示す構成 図である。 disease part 18 of the deep part of the organism tissue 12 via the 2nd optical fibre 10 from the light source for excitation 4 which consists of helium, cadmium laser provided externally.

Since titanium-oxide (TiO2) of the chemical agent for treatments 36 is injected into the deep part of the organism tissue 12, the 442 nm light and the oxidation reduction reaction which were radiated from the excitation source 4 are generated.

The treatment of the disease part 18 of the deep part of the organism tissue 12 will be carried out.

[0043]

(Effect)

Thus in fluorescent observation apparatus 1b of this embodiment, it adds to the effect of the first embodiment like the 2nd embodiment, and disease part 18 treatment of the deep part of the organism tissue 12 is also made.

Moreover, compared with a 2nd embodiment, the light source for treatments and the light source for a diagnosis can use shared one light source, and a size-reduction of the system can be attained.

Furthermore, since it is displayed, using information on the deep part of the organism tissue 12 as an image, diagnostic ability improves.

[0044]

(The 4th embodiment) diagram 6 is a block diagram showing the composition of the fluorescent observation apparatus based on the 4th embodiment of this invention.



[0045]

(構成)図6に示すように、本 実施の形態の蛍光観察装置51 は、被検体の体腔内に挿入する 插入部52の先端部内にMRア ンテナ53を有する内視鏡54 と、内視鏡54に蛍光観察用の 励起光を供給する光源部56a とMRアンテナ53からのMR 信号を増幅するアンプ55とを 備えた光源56と、蛍光観察用 の励起光により励起された生体 組織からの自家蛍光を撮像する イメージインテンシファイヤを 内蔵した高感度カメラ57と、 被検体を静磁場内に置きMRア ンテナ53より高周波磁場を出 カすると共にアンプ55により 増幅されたMRアンテナ53か らのMR信号によりMR画像を 生成するMR画像処理装置58 と、高感度カメラ57により撮 像された撮像信号により蛍光画 像を生成する蛍光画像処理装置 59とを備え、MR画像処理装 置58及び蛍光画像処理装置5 9により生成されたMR画像及 び蛍光画像をモニタ60に表示 するようになっている。

[0046]

[0045]

(Composition)

As shown in a diagram 6, the fluorescent observation apparatus 51 of this embodiment is, the endoscope 54 which has the MR antennae 53 in the end of the insertion part 52 inserted in the intra-corporeal of the subject, the light source 56 equipped with light-source part 56a which supplies the excitation light for fluorescent observation to an endoscope 54, and the amp 55 which amplifies MR signal from the MR antennae 53, the high-sensitivity camera 57 which contained the image intensifier which records the self-fluorescence from the organism tissue excited by the excitation light for fluorescent observation, the MR image processing device 58 which forms MR image with MR signal from the MR antennae 53 amplified with the amp 55 while the subject was placed into the static magnetic field and the high-frequency magnetic field was output from the MR antennae 53, and the fluorescent image processing device 59 which forms a fluorescent image with the image-pickup signal recorded with the high-sensitivity camera 57.

It has these.

MR image formed by the MR image processing device 58 and the fluorescent image processing device 59 and a fluorescent image are displayed in the monitor 60.

[0046]

内視鏡54は、挿入部52の基 For endoscope 54, from holding part 61 端に設けられた把持部61より provided on the base end of an insertion part



源56に着脱自在に延出してお り、光源56からの蛍光観察用 ル62及び挿入部52内に挿通 されたライトガイト63を伝送 し内視鏡54の先端より生体組 織に照射されるようになってい organism tissue. る。

ユニバーサルケーブル62が光 52, the universal cable 62 is extending detachably to light source 56.

The excitation light for the fluorescent の励起光がユニバーサルケーブ observation from a light source 56 transmit the light guide 63 passed through in the universal cable 62 and the insertion part 52, and irradiate from the end of an endoscope 54 to an

[0047]

また、ユニバーサルケーブル**6** 2及び挿入部52内にはMRア ンテナ53に接続された信号線 the MR antennae 53 is arranged. 64が配設されており、この信 号線64によりMRアンテナ5 3からの検出信号が光源56内 this signal line 64. のアンプに伝送されるようにな っている。

[0047]

Moreover, in the universal cable 62 and the insertion part 52, the signal line 64 connected to

The detecting signal from the MR antennae 53 transmits to the amp via light source 56 by

[0048]

さらに、挿入部52及び把持部 が設けられており、蛍光観察用 組織からの自家蛍光を高感度カ メラ57が着脱自在に拍続され る推眼部66に伝送するように なっている。

[0048]

Furthermore, the image guide 65 is provided in 61内にはイメーシカイト65 the insertion part 52 and the holding part 61.

The high-sensitivity camera 57 transmits the の励起光により励起された生体 self-fluorescence from the organism tissue excited by the excitation light for fluorescent observation to the eye-piece part 66 connected detachably.

[0049]

(作用) 次に、このように構成 された本実施の形態の蛍光観察 装置51の作用について説明す る。

[0049]

(Effect)

Next, an effect of the fluorescent observation apparatus 51 of this embodiment constituted in this way is demonstrated.



[0050]

被験体を静磁場内に置き、体腔内に内視鏡54の挿入部52を挿入する。そして、光源56分ら、光額56分の一方が一方がでは、から、大変を出て、光源56分の一方が一方がでは、一方がでは、一方がでは、一方がでは、一方がでは、一方がでは、一方がでは、一方がでは、一方がでは、一方がでは、一方ができる。そのでは、一方ができる。そのでは、一方ができる。そのでは、一方ができる。そのでは、一方ができる。そのでは、一方ができる。そのでは、一方ができる。そのでは、一方ができる。そのでは、一方ができる。というでは、一方ができる。

[0051]

[0050]

被験体を静磁場内に置き、体腔 A subject is placed into a static magnetic field, 内に内視鏡54の挿入部52を and the insertion part 52 of an endoscope 54 is 挿入する。そして、光源56か inserted intra-corporeal.

And, the radiation of the excitation light for fluorescent observation is carried out from a light source 56.

Excitation light is irradiated from the end of an endoscope 54 to an organism tissue via a light quide 63.

An organism tissue's irradiation of excitation light carries out the release of the self-fluorescence from an organism tissue.

This self-fluorescence is sent to the highsensitivity camera 57 via the image guide 65, image processing is carried out by the external fluorescent image processing device 59, and a fluorescent image is displayed by the monitor 60.

[0051]

Moreover, from the MR antennae 53 built-in in the endoscope 54 the MR image processing device 58, the high-frequency signal of a predetermined frequency is sent, and a high-frequency magnetic field is output to the subject from the MR antennae 53.

In addition, as for the direction of this highfrequency magnetic field, it is desirable to cross orthogonally with the direction of the static magnetic field.

And, the MR antennae 53 receive MR signal from a subject, and it is amplified with an amp 55.

がMR画像処理部58に導か Data in the depth direction of the fluorescentれ、モニタ60にMR画像とし disease part currently observed is caught, this



て表示される。

MR signal is guided to MR image-processing part 58, and monitor 60 displays it as a MR image.

[0052]

この結果、術者は、モニタ60 に表示された蛍光画像及びMR 画像により生体の表面、及び深 部方向の観察を行う。

[0053]

(効果) このように本実施の形態の蛍光観察装置51は、病変部の表面の情報が蛍光画像として観察でき、また、病変部の深さ方向の情報がMR画像として観察できるため、生体の表面情報のみならず、深部情報の観察も可能となり、診断能が向上する。

[0054]

(第5の実施の形態)図7及び図8は本発明の第5の実施の形態に係わり、図7は蛍光観察装置の光プローブの構成を示す構成図、図8は図7の光プローブをチャンネルに挿通した内視鏡の構成を示す構成図である。

[0055]

[0052]

Consequently, an operator performs an observation of the surface of the organism, and in the depth direction by the fluorescent image and MR image which were displayed by the monitor 60.

[0053]

(Effect)

Thus information on the surface of a disease part can be observed the fluorescent observation apparatus 51 of this embodiment as a fluorescent image.

観察できるため、生体の表面情 Moreover, since information in the depth 報のみならず、深部情報の観察 direction of the disease part can be observed as a MR image, not only surface information on the organism but an observation of deep-part information is attained, and diagnostic ability improves.

[0054]

(The 5th embodiment) Fig. 7 and 8 is involved in the 5th embodiment of this invention.

Diagram 7 is a block diagram showing the composition of the optical probe of fluorescent observation apparatus. diagram 8 is a block diagram showing the composition of the endoscope which passed through the optical probe of diagram 7 to the channel.

[0055]



第5の実施の形態は、第4の実施の形態とほとんど同じであるので、異なる点のみ説明し、同一の構成には同じ符号をつけ説明は省略する。

[0056] [00

第4の実施の形態では、先端部内にMRアンテナを設けた内視鏡を用いて構成したが、本実施の形態では、通常の内視鏡のチャンネルにMRアンテナを有する光ブローブを挿入して蛍光観察装置を構成する。

[0057]

すなわち、図7に示すように、 本実施の形態における光プロー ブ71は、その内腔に生体組織 からの蛍光画像を伝送するイメ ーシガイト72を内蔵してお り、生体の深部情報を観察する ためにイメージガイト72の外 間に第1のMRアンテナ73 が、また挿入軸方向に沿って第 2のMRアンテナ74がそれぞ れ設けられている。

[0058]

そして、図8に示すように、体腔内に挿入される内視鏡81の チャンネル82内に光プローブ 71を挿通させて先端より突出 させることで、蛍光画像とMR 画像を得るようになっている。 Since the 5th embodiment is almost the same as that of the 4th embodiment, it demonstrates only the different items.

The same code for identical composition is attached and description is omitted.

[0056]

It is constituted from the 4th embodiment using the endoscope which provided MR antennae in the end part.

However, the optical probe which has MR antennae is inserted in the channel of a usual endoscope, and fluorescent observation apparatus consists of this embodiment.

[0057]

That is, as shown in a diagram 7, the optical probe 71 in this embodiment contains the image guide 72 which transmits the fluorescent image from an organism tissue to the lumina.

In order to observe deep-part information on the organism, the first MR antennae 73 is on the periphery of the image guide 72, moreover in the insertion axial direction, the 2nd MR antennae 74 is respectively provided.

[0058]

And, as shown in a diagram 8, a fluorescent image and MR image are obtained by making the optical probe 71 pass through and making it project from an end in the channel 82 of the endoscope 81 inserted intra-corporeal.



[0059]

なお、図示はしないが、第4の 実施の形態と同様に、内視鏡8 1のライトガイト83には光源 56からの蛍光観察用の励起光 が供給され、光プローブフ1の イメージガイドフ2を伝送する 生体組織からの蛍光を高感度か メラ57が撮像し蛍光画像処理 装置59で処理し、さらに第1 のMRアンテナフ3及び第2の MRアンテナ73からのMR信 号をMR画像処理装置58で処 理することで、MR画像処理装 置58及び蛍光画像処理装置5 9により生成されたMR画像及 び蛍光画像をモニタ60亿表示 するようになっている(図6参 照)。

[0060]

(作用) このように構成した本 実施の形態の蛍光観察装置は、 被験体を静磁場内に置き、目的 とする生体内腔に内視鏡81を 挿入する。次に、内視鏡81の チャンネル82内に光ブローブ 71を挿入する。

[0061]

そして、内視鏡81のライトガイト83から、光源56からの 蛍光観察用の励起光を生体組織 に照射する。この励起光の生体 組織への照射により、生体組織 からは自家蛍光が放出される。

[0059]

In addition, it is not illustrated, however, the excitation light for the fluorescent observation from a light source 56 are supplied to the light guide 83 of an endoscope 81 like the 4th embodiment.

The high-sensitivity camera 57 records the fluorescence from the organism tissue which transmits the image guide 72 of the optical probe 71, and it is processed by the fluorescent image processing device 59.

Furthermore by processing MR signal from the first MR antennae 73 and the 2nd MR antennae 73 by the MR image processing device 58, MR image formed by the MR image processing device 58 and the fluorescent image processing device 59 and a fluorescent image are displayed on monitor 60 (diagram 6 reference).

[0060]

(Effect)

Thus the fluorescent observation apparatus of this constituted embodiment puts the subject into a static magnetic field, an endoscope 81 is inserted in a target cavity in the living body, and next, the optical probe 71 is inserted into the channel 82 of an endoscope 81.

[0061]

And from light guide 83 of endoscope 81, the excitation light for the fluorescent observation from a light source 56 are irradiated to an organism tissue.

The release of the self-fluorescence occurs from the organism tissue by the irradiation to



the organism tissue of this excitation light.

[0062]

この自家蛍光は、光プローブ7 1内に設けたイメージガイト7 2を介して高感度カメラ57により撮像され蛍光画像処理装置 59に導かれ、モニタ60に蛍 光画像が表示される。

[0063]

また、光プロープ71に設けた 第1のMRアンテナ73、第2 のMRアンテナ74により得ら れたMR信号をMR画像処理装 置58により処理することで、 3次元のMR画像がモニタ60 に同じく表示される。

[0064]

(効果) このように本実施の形態の蛍光観察装置は、第4実施の形態と比較し、光ブローブ71を内視鏡81のチャンネル82内に挿入し、蛍光観察を行うため、既存の内視鏡81を流用することが可能である。さらに光ブローブ71を使っているため、自由度が大きく任意の位置の病変部が観察可能である。また、MRアンテナを2つ設けてあるため、3次元で生体深部方向の観察可能となる。

[0062]

This self-fluorescence is recorded with the high-sensitivity camera 57 via the image guide 72 provided in the optical probe 71, and is guided to the fluorescent image processing device 59, and a fluorescent image is displayed by monitor 60.

[0063]

Moreover, three-dimensional MR image is similarly displayed by the monitor 60 by processing MR signal obtained with the first MR antennae 73 provided on the optical probe 71, and the 2nd MR antennae 74 by the MR image processing device 58.

[0064]

(Effect)

Thus the fluorescent observation apparatus of this embodiment is compared with the 4th embodiment.

The optical probe 71 is inserted into the channel 82 of an endoscope 81.

することが可能である。さらに Since fluorescent observation is performed, it 光プローブ 7 1 を使っているだ is possible to divert use of the existing め、自由度が大きく任意の位置 endoscope 81.

Furthermore since the optical probe 71 is used, freedom is extensive, and the disease part at arbitrary positions is observeable.

Moreover, since two MR antennae are provided, three-dimensionally in the direction of the organism deep part it can be observed.



[0065]

(第6の実施の形態) 図9ない し図11は本発明の第6の実施 の形態に係わり、図9は蛍光観 察装置の光ブローブをチャンネー ルに挿通した内視鏡の構成を示 す構成図、図10は図9の光ブ ローブをチャンネルに插通した 内視鏡の第1の変形例の構成を 示す構成図、図11は図9の光 プローブをチャンネルに插通し を示す構成図である。

[0066]

第6の実施の形態は、第4の実 施の形態とほとんど同じである ので、異なる点のみ説明し、同 一の構成には同じ符号をつけ説 明は省略する。

[0067]

(構成)第4の実施の形態では、 先端部内にMRアンテナを設け た内視鏡を用いて構成したが、 本実施の形態では、図9に示す ように、第1チャンネル91及 び第2チャンネル92を有する 内視鏡93を用い、生体組織か らの蛍光画像を伝送するイメー

[0065]

(The 6th embodiment) Fig. 9 or 11 is involved in the 6th embodiment of this invention.

Diagram 9 is a block diagram showing the composition of the endoscope which passed through the optical probe of fluorescent observation apparatus to the channel.

Diagram 10 is a block diagram showing the composition of the first modification of the endoscope which passed through the optical た内視鏡の第2の変形例の構成 probe in the diagram 9 to the channel.

> Diagram 11 is a block diagram showing the composition of the 2nd modification of the endoscope which passed through the optical probe in the diagram 9 to the channel.

[0066]

Since the 6th embodiment is almost the same as that of the 4th embodiment, it demonstrates only the different items, the same code for identical composition is attached and description is omitted.

[0067]

(Composition)

It constituted from the 4th embodiment using the endoscope which provided MR antennae to end part.

However, in this embodiment, as shown in a diagram 9, the endoscope 93 which has the 1st channel 91 and the second channel 92 is used. The optical probe 95 which has the image guide シガイト 9 4 を有する光プロー 94 which transmits the fluorescent image from ブタ5を第1チャンネルタ1に an organism tissue is passed through to the 1st 插通し、MRアンテナ96を有 channel 91, and a fluorescent observation



するMRプローブ97を第2チ ヤンネルタ2に挿通することで 蛍光観察装置を構成する。

apparatus consists of passing through the MR probe 97 which has the MR antennae 96, to the second channel 92.

[0068]

なお、図示はしないが、第4の 実施の形態と同様に、内視鏡の 3のライトガイト98には光源 56からの蛍光観察用の励起光 が供給され、光ブローブ95の イメージガイド94を伝送する 生体組織からの蛍光を高感度か メラ57が撮像し蛍光画像処理 装置59で処理し、さらにMR アンテナタ6からのMR信号を MR画像処理装置58で処理す ることで、MR画像処理装置5 8及び蛍光画像処理装置59に より生成されたMR画像及び蛍 光画像をモニタ60に表示する ようになっている(図6参照)。

[0069]

(作用) このように構成した本 実施の形態の蛍光観察装置は、 被検体を静磁場内に置き、目的 とする生体内腔に内視鏡93を 挿入する。次に、内視鏡93の 第1チャンネル91内に光プロ ープ95を挿入し、第2チャン ネル92内にMRプローブ97 を挿入する。

[0070]

[0068]

In addition, while it is not illustrated, the excitation light for the fluorescent observation from a light source 56 is supplied to the light guide 98 of an endoscope 93 like in the 4th embodiment.

The high-sensitivity camera 57 records the fluorescence from the organism tissue which transmits the image guide 94 of the optical probe 95, and it is processed by the fluorescent image processing device 59.

Furthermore by processing MR signal from the MR antennae 96 by the MR image processing device 58, MR image formed by the MR image processing device 58 and the fluorescent image processing device 59 and a fluorescent image are displayed in the monitor 60 (diagram 6 reference).

[0069]

(Effect)

Thus the fluorescent observation apparatus of this constituted embodiment puts the subject into a static magnetic field, an endoscope 93 is inserted in the target cavity in the living body, next, the optical probe 95 is inserted into 1st channel 91 of an endoscope 93, and the MR probe 97 is inserted into the second channel 92.

[0070]

そして、内視鏡93のライトガ And from light guide 98 of endoscope 93, the



イド98から、光源56からの 蛍光観察用の励起光を生体組織 に照射する。この励起光の生体 組織への照射により、生体組織 からは自家蛍光が放出される。

excitation light for the fluorescent observation from a light source 56 are irradiated to an organism tissue.

The release of the self-fluorescence occurs from the organism tissue by the irradiation to the organism tissue of this excitation light.

[0071]

この自家蛍光は、光プローブ9 5内に設けたイメージガイド9 4を介して高感度カメラ57に より撮像され蛍光画像処理装置 59に導かれ、モニタ60に蛍 光画像が表示される。

[0072]

また、MRプローブ97に設け たMRアンテナ96により得ら れたMR信号をMR画像処理装 置58により処理することで、 **MR画像がモニタ60**に同じく device 58. 表示される。

[0073]

(効果) 本実施の形態において (Effect) も、第4の実施の形態と同様に、 病変部の表面の情報が蛍光画像 として観察でき、また、病変部 の深さ方向の情報がMR画像と して観察できるため、生体の表 面情報のみならず、深部情報の 観察も可能となり、診断能が向 上する。

[0074]

[0071]

This self-fluorescence is recorded with the high-sensitivity camera 57 via the image guide 94 provided in the optical probe 95, and is guided to the fluorescent image processing device 59, and a fluorescent image is displayed by the monitor 60.

[0072]

Moreover, MR image is similarly displayed by the monitor 60 by processing MR signal obtained with the MR antennae 96 provided on the MR probe 97 by the MR image processing

[0073]

Also in this embodiment, information on the surface of a disease part can be observed as a fluorescent image like the 4th embodiment.

Moreover, since data in the depth direction of a disease part can be observed as a MR image, not only surface information on the organism but an observation of deep-part information is attained, and diagnostic ability improves.

[0074]

なお、MRプローブ97の代わ In addition, instead of the MR probe 97, an



深部精報の観察を行ってもよ information may be observed. U.

りに、超音波プローブを用いて ultrasonic probe may be used and deep-part

[0075]

また、図9に示した第1チャン ネルタ1及び第2チャンネルタ 2を有する内視鏡93の代わり に、図10に示すように、内径 の太い大チャンネル101を有 する内視鏡102を用いて蛍光 観察装置を構成してもよく、こ の場合、大チャンネル101に された半円状のMRプローブ1 04及びイメージガイド105 が插通された半円状の光プロー ブ106が挿入される。このよ うな構成でも本実施の形態と同 様な作用・効果を得ることがで きる。

[0076]

さらに、内視鏡102の大チャ ンネル101に、図11に示す ように、MRアンテナ103を 内蔵する中空状のMRプローブ 111を挿入すると共に、前記 MRプローブ111の中空部に イメージガイド105を内蔵す る光プローブ112が挿入し蛍 光観察装置を構成しても、本実 施の形態と同様な作用・効果を 得ることができる。

[0077]

[0075]

Moreover, instead of the endoscope 93 which has the 1st channel 91 and the second channel 92 which were shown in a diagram 9, as shown in a diagram 10, fluorescent observation apparatus may be constituted using the endoscope 102 which has the large channel 101 with a thick internal diameter.

In this case, the semicircle-shaped optical は、MRアンテナ103が挿通 probe 106 with which the semicircle-like MR probe 104 with which the MR antennae 103 were passed through, and the image guide 105 were passed through is inserted in the large channel 101, and the same effect of this embodiment can be obtained.

[0076]

As shown in a diagram 11, while inserting in the large channel 101 of an endoscope 102 the hollow MR probe 111 which contains the MR antennae 103, furthermore, even if the optical probe 112 which contains the image guide 105 in the hollow part of the above-mentioned MR probe 111 inserts and it constitutes fluorescent observation apparatus, the same effect as this embodiment can be obtained.

[0077]



(第7の実施の形態)図12は 本発明の第7の実施の形態に係る蛍光観察装置の構成を示す構 放図である。

(The 7th embodiment) diagram 12 is a block diagram showing the composition of the fluorescent observation apparatus based on the 7th embodiment of this invention.

[0078]

(構成) 本実施の形態は、外科 処置に蛍光観察を応用したもの であり、図12に示すように、 腹壁120を介して体腔内に挿 入される硬性な挿入部121を 有する硬性内視鏡122におい て、挿入部121の基端に連設 されている把持部123には、 挿入部121内に配設された第 1のチャンネル及び第2のチャ ンネル(図示せず)に連通した 第1のチャンネルロ金124及 び第1のチャンネルロ金125 が設けられ、把持部123亿設 けられた接眼部126にはイメ ージインテンシファイヤを内蔵 した高感度カメラ127が着脱 自在に拍続される。

[0079]

そして、本実施の形態の蛍光観察装置130は、前記硬性内視鏡122と、高感度カメラ127からの信号を信号処理しモニタ131に蛍光画像を表示する蛍光画像処理装置132と、把持部123に拍続され蛍光観察を行うために励起光を前記硬性内視鏡122に供給する励起用光源133と、第1のチャンネ

[0078]

(Composition)

This embodiment applies fluorescent observation to a surgery treatment.

In the hard endoscope 122 which has the hard insertion part 121 inserted intra-corporeal via abdominal wall 120 as shown in a diagram 12, the first channel metal_collet 124 and the first channel metal_collet 125 which were connected to the first channel and the 2nd channel (not shown) which were arranged in the insertion part 121 are provided in the holding part 123 currently articulated by the base end of insertion part 121.

The high-sensitivity camera 127 which contained the image intensifier is detachably connected to the eye-piece part 126 provided in the holding part 123.

[0079]

And, for the fluorescent observation apparatus 130 of this embodiment, the above-mentioned hard endoscope 122, the fluorescent image processing device 132 which carries out the signal processing of the signal from the high-sensitivity camera 127, and displays a fluorescent image to a monitor 131, the light source for excitation 133 which supplies excitation light to the above-mentioned hard endoscope 122 in order to connect with the



ルロ金124から第1のチャン ネルに挿入される病変部134 を処置するための超音波破砕プ ローブ135を制御する処置具 制御装置136と、第2のチャ ンネルにより第2のチャンネル 口金125を介して破砕した組 備えて構成される。

holding part 123 and to perform fluorescent observation, the treatment-tool apparatus 136 which controls the ultrasonic crushing probe 135 for carrying out the treatment of the disease part 134 inserted in a first channel from the first channel metal_collet 124, and the recovery bottle 137 which recovers 織を回収する回収瓶137とを the tissue crushed via the 2nd channel metal collet 125 by the 2nd channel. It has these and it is constituted.

[0080]

(作用) 硬性内視鏡 1 2 2 の挿 (Effect) 入部121を腹壁120を介し て体腔内に插入する。そして、 励起用光源 133から蛍光観察 wall 120. 用の励起光を硬性内視鏡122 介して腹腔内に照射する。する と、腹腔内の臓器の病変部 13 4からは自家蛍光が放出され、 硬性内視鏡122のイメージガ イド(図示せず)を介して自家 蛍光が高感度カメラ127に伝 organ in the abdominal cavity. 送される。そして、蛍光画像処 後、モニタ131に病変部13 4の蛍光画像が表示される。

[0800]

The insertion part 121 of the hard endoscope 122 is inserted intra-corporeal via abdominal

And, the excitation light for fluorescent のライトガイト(図示せず)を observation is irradiated in the abdominal cavity via the light guide (not shown) of the hard endoscope 122 from the light source for excitation 133.

> Then, the release of the self-fluorescence is carried out from the disease part 134 of the

A self-fluorescence is transmitted to the high-理装置132で画像処理された sensitivity camera 127 via the image guide (not shown) of the hard endoscope 122.

> And, after image processing fluorescent image processing device 132, the fluorescent image of the disease part 134 is displayed by the monitor 131.

[0081]

[0081]

術者はモニタ 13 1 に表示され After the operator observed the permeation た蛍光画像により、病変部の浸 extent of the disease part by the fluorescent 潤度合いを観察した後、第1の image displayed by the monitor 131, the



チャンネルロ金124より第1 のチャンネルに挿入した超音波 破砕プローブ135及び処置具 制御装置136を操作して、病 変部134を破砕する。破砕さ れた病変組織は硬性内視鏡12 第2のチャンネルロ金125よ り外部の回収瓶 1 3 7 に回収さ the hard endoscope 122. れる。

ultrasonic crushing probe 135 treatment-tool control apparatus 136 which were inserted in the first channel from the first channel metal_collet 124 are operated, and the disease part 134 is crushed.

The crushed lesioned tissue is recovered by 2の第2のチャンネルを介して the external recovery bottle 137 from the 2nd channel metal_collet 125 via the 2nd channel of

[0082]

(効果) このように、本実施の 形態の蛍光観察装置130で は、腹腔内の病変部134の位 置確認、浸潤範囲の確認が容易 となるため、治療を確実に行う ことができる。

[0082]

(Effect)

In this way, it is with the fluorescent observation apparatus 130 of this embodiment. Since locating the disease part 134 in an abdominal cavity and to confirm the permeation extent becomes easy, treatment can be performed reliably.

[0083]

[0083]

【付記】

(付記項1) 生体組織に励起 光を照射し、前記生体組織から 発生する蛍光により前記生体組 織を観察する蛍光観察装置にお いて、生体深部組織に穿刺する 針状シースと、前記針状シース の前記生体深部組織への穿刺状 態を確認する超音波観察手段と を備え、前記針状シースの内部 に前記励起光を伝送する照明用 光ファイバと、前記生体組織か ら発生する蛍光を伝送する観察 sheath.

[Additional remark]

(Additional-remark item 1) Excitation light is irradiated to an organism tissue.

In the fluorescent observation apparatus which observes the above-mentioned organism tissue according to the fluorescence generated from the above-mentioned organism tissue, it has the needle-like sheath transfixed to an organism deep-part tissue and ultrasonic observation means to confirm the transfix state to the above-mentioned organism deep-part tissue of the above-mentioned needle-like



用光ファイバとを設けたことを 特徴とする蛍光観察装置。 The optical fibre for illumination which transmits above-mentioned excitation light inside the above-mentioned needle-like sheath, and the optical fibre for observation which transmits the fluorescence generated from the above-mentioned organism tissue were provided.

The fluorescent observation apparatus characterized by the above-mentioned.

[0084]

(付記項2) 前記照明用光ファイバを介して照射した前記励起光に反応を起こす薬剤で前記生体深部組織の病変部を治療する治療手段を備えたことを特徴とする付記項1に記載の蛍光観察装置。

[0084]

(Additional-remark item 2) It had treatment means which carries out the treatment of the disease part of the above-mentioned organism deep-part tissue to the above-mentioned excitation light which irradiated via the above-mentioned optical fibre for illumination, with the chemical agent which undergoes reaction.

The fluorescent observation apparatus of the additional-remark item 1 characterized by the above-mentioned.

[0085]

(付記項3) 前記薬剤はPD (Additional-rei T用の薬剤であることを特徴と mentioned ch する付記項2に記載の蛍光観察 for PDT. 装置。 The fluores

[0085]

(Additional-remark item 3) An abovementioned chemical agent is a chemical agent for PDT.

The fluorescent observation apparatus of the additional-remark item 2 characterized by the above-mentioned.

[0086]

(付記項4) 前記薬剤はルミンであることを特徴とする付記項2に記載の蛍光観察装置。

[0086]

(Additional-remark item 4) An above-mentioned chemical agent is ?lumine?.

The fluorescent observation apparatus of the additional-remark item 2 characterized by the above-mentioned.



[0087]

(付記項5) 前記薬剤はTi O 2 であることを特徴とする 付記項2に記載の蛍光観察装 置。

[0087]

(Additional-remark item 5) An abovementioned chemical agent is TiO2.

The fluorescent observation apparatus of the additional-remark item 2 characterized by the above-mentioned.

[8800]

[8800]

【発明の効果】

以上説明したように本発明の蛍 As explained above, 光観察装置によれば、針状シー スを生体深部組織に穿刺し、超 音波観察手段により針状シース の生体深部組織への穿刺状態を 確認すると共に、照明用光ファ イバにより生体組織に励起光を 伝送し、観察用光ファイバによ り前記生体組織から発生する蛍 光を伝送するので、生体の深部 に存在する病変部の観察を行う ことできるという効果がある。

[EFFECT OF THE INVENTION]

according the fluorescent observation apparatus this invention, a needle-like sheath is transfixed to an organism deep-part tissue.

While confirming the transfix state to the organism deep-part tissue of a needle-like sheath by ultrasonic observation means. excitation light is transmitted to an organism tissue by the optical fibre for illumination.

Since the fluorescence generated from the above-mentioned organism tissue by the optical fibre for observation is transmitted, the disease part which exists in a deep part of the organism can be observed.

The above-mentioned effect is expectable.

【図面の簡単な説明】

[BRIEF EXPLANATION OF DRAWINGS]

【図1】

成図

[FIGURE 1]

本発明の第1の実施の形態に係 The block diagram showing the composition of る蛍光観察装置の構成を示す構 the fluorescent observation apparatus based on the first embodiment of this invention



[図2]

図1の光ブローブを插通する蛍 光観察装置に用いられるコンベ ックス型超音波内視鏡の構成を 示す構成図

[図3]

図2のコンペックス型超音波内 視鏡により得られた超音波画像 を表示するモニタを示す図で

【図4】

本発明の第2の実施の形態に係 る蛍光観察装置の構成を示す構 成図

[図5]

本発明の第3の実施の形態に係 る蛍光観察装置の構成を示す構 成図

【図6】

成図

[図7]

る蛍光観察装置の光プローブの 構成を示す構成図

[図8]

[FIGURE 2]

The block diagram showing the composition of the convex type ultrasound endoscopy used for the fluorescent observation apparatus which passes through the optical probe of diagram 1

[FIGURE 3]

The diagram showing the monitor which displays the ultrasonic image obtained by the convex type ultrasound endoscopy of diagram 2.

[FIGURE 4]

The block diagram showing the composition of the fluorescent observation apparatus based on the 2nd embodiment of this invention

[FIGURE 5]

The block diagram showing the composition of the fluorescent observation apparatus based on the third embodiment of this invention

[FIGURE 6]

本発明の第4の実施の形態に係 The block diagram showing the composition of る蛍光観察装置の構成を示す構 the fluorescent observation apparatus based on the 4th embodiment of this invention

[FIGURE 7]

本発明の第5の実施の形態に係 The block diagram showing the composition of the optical probe of the fluorescent observation apparatus based on the 5th embodiment of this invention

[FIGURE 8]

図7の光プローブをチャンネル The block diagram showing the composition of に挿通した内視鏡の構成を示す the endoscope which passed through the



構成図

[図9]

本発明の第6の実施の形態に係る蛍光観察装置の光ブローブを チャンネルに挿通した内視鏡の 構成を示す構成図

【図10】

図 9 の光プローブをチャンネル に插通した内視鏡の第 1 の変形 例の構成を示す構成図

[図11]

図 9 の光プローブをチャンネル に挿通した内視鏡の第 2 の変形 例の構成を示す構成図

【図12】

本発明の第7の実施の形態に係る蛍光観察装置の構成を示す構成図

【符号の説明】

1…蛍光観察装置

2…シース

3…光プローブ

4…励起用光源

5…制御装置

6…スペクトロメータ

7…第1チャンネル

8…第2チャンネル

9…第1の光ファイバ

optical probe in the diagram 7 to the channel

[FIGURE 9]

The block diagram showing the composition of the endoscope which passed through the optical probe of the fluorescent observation apparatus based on the 6th embodiment of this invention to the channel

[FIGURE 10]

The block diagram showing the composition of the first modification of the endoscope which passed through the optical probe in the diagram 9 to the channel

[FIGURE 11]

The block diagram showing the composition of the 2nd modification of the endoscope which passed through the optical probe in the diagram 9 to the channel

[FIGURE 12]

The block diagram showing the composition of the fluorescent observation apparatus based on the 7th embodiment of this invention

[EXPLANATION OF DRAWINGS]

1... fluorescence observation apparatus

2... sheath

3... light probe

Light source for excitation

5... control apparatus

6... spectrometer

7... The 1st channel

8... second channel

9... first optical fibre



10…第2の光ファイバ

10... 2nd optical fibre

1 1 …先端部

11... end

12…生体組織

12... organism tissue

13…対物光学系

13... object optical system

14…超音波送受信部

14... ultrasonic-wave transmitting-and-receiving

15…コンペックス型超音波内

part

視鏡

15... convex type ultrasound endoscopy

16…チャンネル

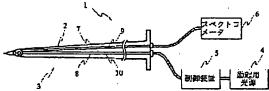
16... channel

17…外部モニタ

17... external monitor

[図1]

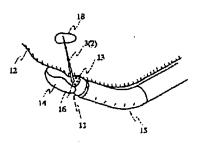
[FIGURE 1]



refer to EXPLANATION OF DRAWINGS

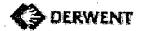
[図2]

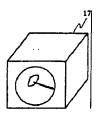
[FIGURE 2]



[図3]

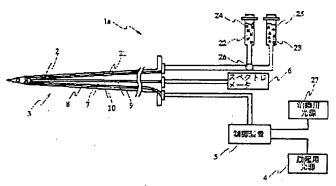
[FIGURE 3]





【図4】

[FIGURE 4]

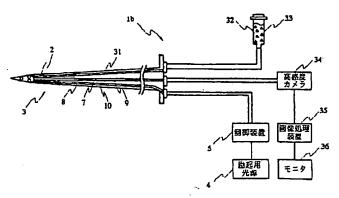


[translation of Japanese text in Figure 4] refer to EXPLANATION OF DRAWINGS 27 therapeutic light source

[図5]

[FIGURE 5]





[translation of Japanese text in Figure 5] refer to EXPLANATION OF DRAWINGS

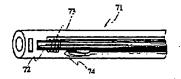
34 highly sensitive camera

35 image processing unit

36 monitor

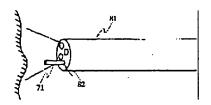
【図7】

[FIGURE 7]



[図8]

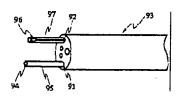
[FIGURE 8]





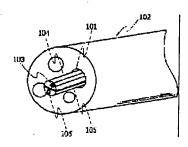
[図9]

[FIGURE 9]



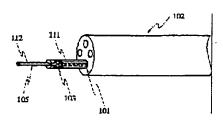
[図10]

[FIGURE 10]



【図11】

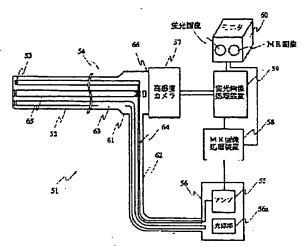
[FIGURE 11]



【図6】

[FIGURE 6]





[translation of Japanese text in Figure 6] refer to EXPLANATION OF DRAWINGS

	l
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J	I CALL LU

56a light source

57 highly sensitive camera

58 MR image processing unit

59 fluorescent image processing unit

60 monitor

60 left circle fluorescent imag

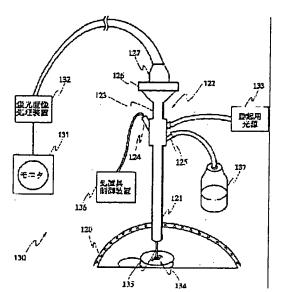
60 right circle MR image

[図12]

[FIGURE 12]

JP11-155812-A





[translation of Japanese text in Figure 12] refer to EXPLANATION OF DRAWINGS

131 monitor

132 fluorescent image processing unit

133 excitation light source

136 tool control unit



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